

2 **The protonmotive force and respiratory control:**

3 **Building blocks of mitochondrial physiology**

4 **Part 1.**

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**Updates:**

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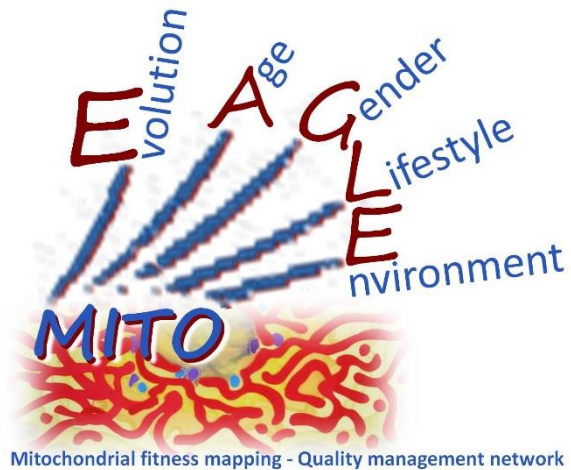
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This manuscript on 'The protonmotive force and respiratory control' is a position statement in the frame of COST Action CA15203 MitoEAGLE. The list of co-authors evolved from MitoEAGLE Working Group Meetings and a **bottom-up** spirit of COST in phase 1: This is an open invitation to scientists and students to join as co-authors, to provide a balanced view on mitochondrial respiratory control, a fundamental introductory presentation of the concept of the protonmotive force, and a consensus statement on reporting data of mitochondrial respiration in terms of metabolic flows and fluxes. We plan a series of follow-up reports by the expanding MitoEAGLE Network, to increase the scope of recommendations on harmonization and facilitate global communication and collaboration.



**Phase 2: MitoEAGLE preprint (Versions 01 – 10):** We continue to invite comments and suggestions on the, particularly if you are an **early career investigator adding an open future-oriented perspective**, or an **established scientist providing a balanced historical basis**. Your critical input into the quality of the manuscript will be most welcome, improving our aims to be educational, general, consensus-oriented, and practically helpful for students working in mitochondrial respiratory physiology.

**Phase 3 (2017-11-11): Manuscript submission to a preprint server, such as BioRxiv.** We want to invite further opinion leaders: To join as a co-author, please feel free to focus on a particular section in terms of direct input and references, contributing to the scope of the manuscript from the perspective of your expertise. Your comments will be largely posted on the discussion page of the MitoEAGLE preprint website.

If you prefer to submit comments in the format of a referee's evaluation rather than a contribution as a co-author, I will be glad to distribute your views to the updated list of co-authors for a balanced response. We would ask for your consent on this open bottom-up policy.

**Phase 4:** We organize a MitoEAGLE session linked to our series of reports at the MiPconference Nov 2017 in Hradec Kralove in close association with the MiPsociety (where you hopefully will attend) and at EBEC 2018 in Budapest.

» [http://www.mitoeagle.org/index.php/MiP2017\\_Hradec\\_Kralove\\_CZ](http://www.mitoeagle.org/index.php/MiP2017_Hradec_Kralove_CZ)

I thank you in advance for your feedback.

With best wishes,

Erich Gnaiger

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144 **Abstract**

145 Clarity of concept and consistency of nomenclature are key trademarks of a research field.  
146 These trademarks facilitate effective transdisciplinary communication, education, and  
147 ultimately further discovery. As the knowledge base and importance of mitochondrial  
148 physiology to human health expand, the necessity for harmonizing nomenclature concerning  
149 mitochondrial respiratory states and rates has become increasingly apparent. Peter Mitchell's  
150 concept of the protonmotive force establishes the links between electrical and chemical  
151 components of energy transformation and coupling in oxidative phosphorylation. This unifying  
152 concept provides the framework for developing a consistent nomenclature for mitochondrial  
153 physiology and bioenergetics. Herein, we follow IUPAC guidelines on general terms of  
154 physical chemistry, extended by the concepts of open systems and irreversible thermodynamics.  
155 We align the nomenclature of classical bioenergetics on respiratory states with a concept-driven  
156 constructive terminology to address the meaning of each respiratory state. Furthermore, we  
157 suggest uniform standards for the evaluation of respiratory states that will ultimately support  
158 the development of databases of mitochondrial respiratory function in species, tissues and cells  
159 studied under diverse physiological and experimental conditions. In this position statement, in  
160 the frame of COST Action CA15203 MitoEAGLE, we endeavour to provide a balanced view  
161 on mitochondrial respiratory control, a fundamental introductory presentation of the concept of  
162 the protonmotive force, and a critical discussion on reporting data of mitochondrial respiration  
163 in terms of metabolic flows and fluxes.

164

165 *Keywords:* Mitochondrial respiratory control, coupling control, mitochondrial  
166 preparations, protonmotive force, chemiosmotic theory, oxidative phosphorylation, OXPHOS,  
167 efficiency, electron transfer, ET; proton leak, LEAK, residual oxygen consumption, ROX, State  
168 2, State 3, State 4, normalization, flow, flux

169

170

171 **Box 1:**

172

173 **In brief:**174 **mitochondria**175 **and Bioblasts**

- \* Does the public expect biologists to understand Darwin's theory of evolution?
- \* Do students expect that researchers of bioenergetics can explain Mitchell's theory of chemiosmotic energy transformation?

176 **Mitochondria** were described for the first time in 1857 by Rudolph Albert Kölliker as granular177 structures or 'sarkosomes' (*a reference is needed*). In 1886 (*a reference is needed*) Richard

178 Altmann called them 'bioblasts' (published 1894). The word 'mitochondrium' (Greek mitos:

179 thread; chondros: granule) was introduced by Carl Benda (1898). Mitochondria are the oxygen

180 consuming electrochemical generators which evolved from endosymbiotic bacteria (Margulis

181 1970; Lane 2005). The bioblasts of Richard Altmann (1894) included not only the mitochondria

182 as presently defined, but also symbiotic and free-living bacteria.

183 We now recognize mitochondria as dynamic organelles with a double membrane that are

184 contained within eukaryotic cells. The mitochondrial inner membrane (mtIM) shows dynamic

185 tubular to disk-shaped cristae that separate the mitochondrial matrix, *i.e.* the internal

186 mitochondrial compartment, and the intermembrane space; the latter being enclosed by the

187 mitochondrial outer membrane (mtOM). Mitochondria are the structural and functional

188 elemental units of cell respiration. Cell respiration is the consumption of oxygen by electron

189 transfer coupled to electrochemical proton translocation across the mtIM. In the process of

190 oxidative phosphorylation (OXPHOS), the reduction of O<sub>2</sub> is electrochemically coupled to the

191 transformation of energy in the form of adenosine triphosphate (ATP; Mitchell 2011). These

192 powerhouses of the cell contain the machinery of the OXPHOS-pathway, including

193 transmembrane respiratory complexes (*i.e.* proton pumps with FMN, Fe-S and cytochrome *b*,194 *c*, *aa*<sub>3</sub> redox systems); alternative dehydrogenases and oxidases; the coenzyme ubiquinone (Q);

195 ATP synthase; the enzymes of the tricarboxylic acid cycle and the fatty acid oxidation enzymes;

196 transporters of ions, metabolites and co-factors; and mitochondrial kinases related to energy

197 transfer pathways. The mitochondrial proteome comprises over 1,200 proteins

198 (MITOCARTA), mostly encoded by nuclear DNA (nDNA), with a variety of functions, many  
199 of which are relatively well known (*e.g.* apoptosis-regulating proteins), while others are still  
200 under investigation, or need to be identified (*e.g.* alanine transporter).

201 Mitochondria typically maintain several copies of their own genome (hundred to  
202 thousands per cell; Cummins 1998), which is almost exclusively maternally inherited (White *et*  
203 *al.* 2008) and known as mitochondrial DNA (mtDNA). One exception to strictly maternal  
204 inheritance in animals is found in bivalves (Breton *et al.* 2007). mtDNA is 16.5 Kb in length,  
205 contains 13 protein-coding genes for subunits of the transmembrane respiratory Complexes CI,  
206 CIII, CIV and ATP synthase, and also encodes 22 tRNAs and the mitochondrial 16S and 12S  
207 rRNA. The mitochondrial genome is both regulated and supplemented by nuclear-encoded  
208 mitochondrial targeted proteins. Evidence has accumulated that additional gene content is  
209 encoded in the mitochondrial genome, *e.g.* microRNAs, piRNA, smithRNAs, repeat associated  
210 RNA, and even additional proteins (Duarte *et al.* 2014; Lee *et al.* 2015; Cobb *et al.* 2016).

211 The mtIM contains the non-bilayer phospholipid cardiolipin, which is not present in any  
212 other eukaryotic cellular membrane. Cardiolipin promotes the formation of respiratory  
213 supercomplexes, which are supramolecular assemblies based upon specific, though dynamic,  
214 interactions between individual respiratory complexes (Greggio *et al.* 2017; Lenaz *et al.* 2017).  
215 Membrane fluidity is an important parameter influencing functional properties of proteins  
216 incorporated in the membranes (Waczulikova *et al.* 2007). There is a constant crosstalk between  
217 mitochondria and the other cellular components, maintaining cellular mitostasis through  
218 regulation at both the transcriptional and post-translational level, and through cell signalling  
219 including proteostatic (*e.g.* the ubiquitin-proteasome and autophagy-lysosome pathways) and  
220 genome stability modules throughout the cell cycle or even cell death, contributing to  
221 homeostatic regulation in response to varying energy demands and stress (Quiros *et al.* 2016).  
222 In addition to mitochondrial movement along the microtubules, mitochondrial morphology can  
223 change in response to the energy requirements of the cell via processes known as fusion and

224 fission, through which mitochondria can communicate within a network, and in response to  
225 intracellular stress factors causing swelling and ultimately permeability transition.

226 Mitochondrial dysfunction is associated with a wide variety of genetic and degenerative  
227 diseases. Robust mitochondrial function is supported by physical exercise and caloric balance,  
228 and is central for sustained metabolic health throughout life. Therefore, a better understanding  
229 of mitochondrial physiology will improve our understanding of the etiology of disease, the  
230 diagnostic repertoire of mitochondrial medicine, with a focus on protective medicine, lifestyle  
231 and healthy aging.

232 Abbreviation: mt, as generally used in mtDNA. Mitochondrion is singular and  
233 mitochondria is plural.

234 *‘For the physiologist, mitochondria afforded the first opportunity for an experimental*  
235 *approach to structure-function relationships, in particular those involved in active transport,*  
236 *vectorial metabolism, and metabolic control mechanisms on a subcellular level’ (Ernster and*  
237 *Schatz 1981).*

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238

## 239 **1. Introduction**

240 Mitochondria are the powerhouses of the cell with numerous physiological, molecular,  
241 and genetic functions (**Box 1**). Every study of mitochondrial function and disease is faced with  
242 **E**volution, **A**ge, **G**ender and sex, **L**ifestyle, and **E**nvironment (EAGLE) as essential background  
243 conditions intrinsic to the individual patient or subject, cohort, species, tissue and to some extent  
244 even cell line. As a large and highly coordinated group of laboratories and researchers, the  
245 mission of the global MitoEAGLE Network is to generate the necessary scale, type, and quality  
246 of consistent data sets and conditions to address this intrinsic complexity. Harmonization of  
247 experimental protocols and implementation of a quality control and data management system  
248 is required to interrelate results gathered across a spectrum of studies and to generate a  
249 rigorously monitored database focused on mitochondrial respiratory function. In this way,



250 researchers within the same and across different disciplines will be positioned to compare their  
251 findings to an agreed upon set of clearly defined and accepted international standards.

252 Reliability and comparability of quantitative results depend on the accuracy of  
253 measurements under strictly-defined conditions. A conceptually defined framework is also  
254 required to warrant meaningful interpretation and comparability of experimental outcomes  
255 carried out by research groups at different institutes. With an emphasis on quality of research,  
256 collected data can be useful far beyond the specific question of a particular experiment.  
257 Enabling meta-analytic studies is the most economic way of providing robust answers to  
258 biological questions (Cooper *et al.* 2009). Vague or ambiguous jargon can lead to confusion  
259 and may relegate valuable signals to wasteful noise. For this reason, measured values must be  
260 expressed in standardized units for each parameter used to define mitochondrial respiratory  
261 function. Standardization of nomenclature and definition of technical terms is essential to  
262 improve the awareness of the intricate meaning of a divergent scientific vocabulary. The focus  
263 on the protonmotive force, coupling states, and fluxes through metabolic pathways of aerobic  
264 energy transformation in mitochondrial preparations is a first step in the attempt to generate a  
265 harmonized and conceptually-oriented nomenclature in bioenergetics and mitochondrial  
266 physiology. Coupling states of intact cells and respiratory control by fuel substrates and specific  
267 inhibitors of respiratory enzymes will be reviewed in subsequent communications.

268

## 269 **2. Respiratory coupling states in mitochondrial preparations**

270 *‘Every professional group develops its own technical jargon for talking about*  
271 *matters of critical concern ... People who know a word can share that idea with*  
272 *other members of their group, and a shared vocabulary is part of the glue that holds*  
273 *people together and allows them to create a shared culture’ (Miller 1991).*

274

275           **Mitochondrial preparations** are defined as either isolated mitochondria, or tissue and  
276 cellular preparations in which the barrier function of the plasma membrane is disrupted. The  
277 plasma membrane separates the cytosol, nucleus, and organelles (the intracellular  
278 compartment) from the environment of the cell. The plasma membrane consists of a lipid  
279 bilayer, embedded proteins, and attached organic molecules that collectively control the  
280 selective permeability of ions, organic molecules, and particles across the cell boundary. The  
281 intact plasma membrane, therefore, prevents the passage of many water-soluble mitochondrial  
282 substrates, such as succinate or adenosine diphosphate (ADP), that are required for the analysis  
283 of respiratory capacity at kinetically-saturating concentrations, thus limiting the scope of  
284 investigations into mitochondrial respiratory function in intact cells. The cholesterol content of  
285 the plasma membrane is high compared to mitochondrial membranes. Therefore, mild  
286 detergents, such as digitonin and saponin, can be applied to selectively permeabilize the plasma  
287 membrane by interaction with cholesterol and allow free exchange of cytosolic components  
288 with ions and organic molecules of the immediate cell environment, while maintaining the  
289 integrity and localization of organelles, cytoskeleton, and the nucleus. Application of optimum  
290 concentrations of these mild detergents leads to the complete loss of cell viability, tested by  
291 nuclear staining, while mitochondrial function remains intact, as shown by an unaltered  
292 respiration rate of isolated mitochondria after the addition of such low concentrations of digitonin  
293 and saponin. In addition to mechanical permeabilization during homogenization of fresh tissue,  
294 saponin may be applied to ensure permeabilization of all cells. Crude homogenate and cells  
295 permeabilized in the respiration chamber contain all components of the cell at highly diluted  
296 concentrations. All mitochondria are retained in chemically-permeabilized mitochondrial  
297 preparations and crude tissue homogenates. In the preparation of isolated mitochondria, the  
298 cells or tissues are homogenized, and the mitochondria are separated from other cell fractions  
299 and purified by differential centrifugation, entailing the loss of a significant fraction of

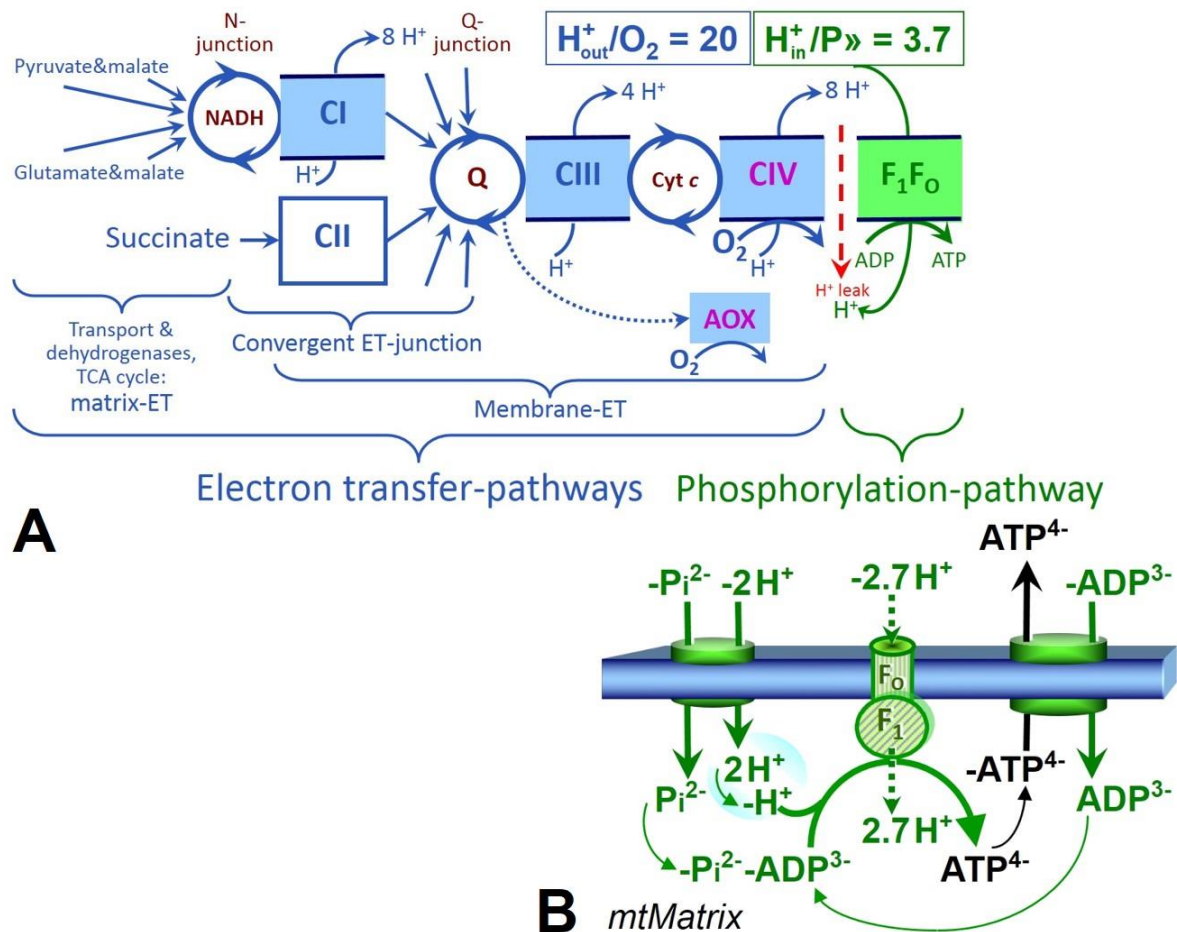
300 mitochondria. The term mitochondrial preparation does not include further fractionation of  
301 mitochondrial components, as well as submitochondrial particles.

302

### 303 *2.1. Three coupling states of mitochondrial preparations and residual oxygen consumption*

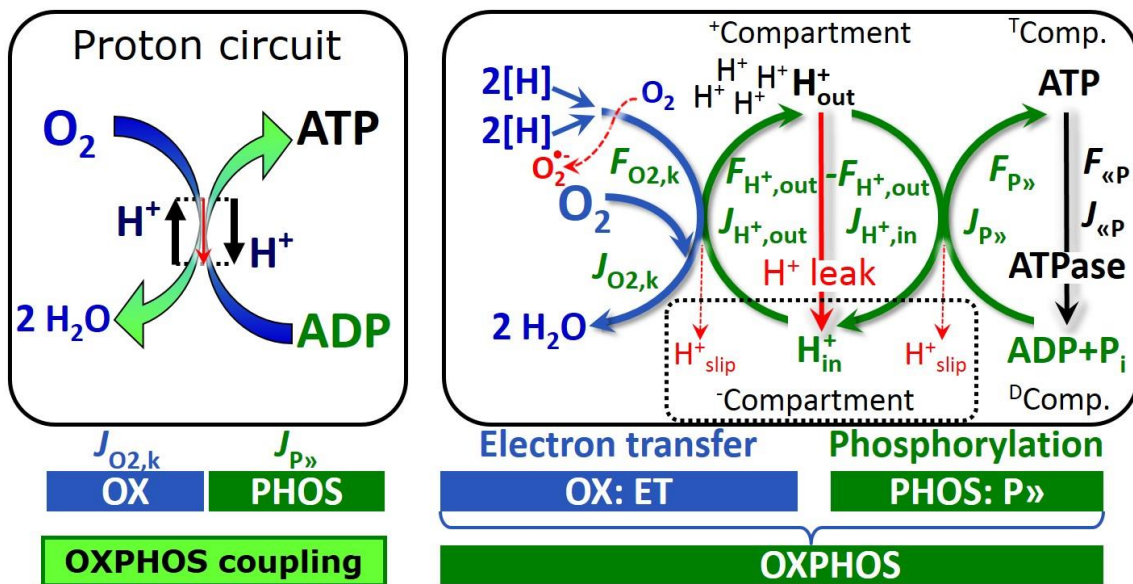
304 **Respiratory capacities in coupling control states:** To extend the classical nomenclature  
305 on mitochondrial coupling states (Section 2.4) by a concept-driven terminology that  
306 incorporates explicit information on the nature of the respiratory states, the terminology must  
307 be general and not restricted to any particular experimental protocol or mitochondrial  
308 preparation (Gnaiger 2009). We focus primarily on the conceptual ‘why’, along with  
309 clarification of the experimental ‘how’. In the following section, the concept-driven  
310 terminology is explained and coupling states are defined. We define respiratory capacities,  
311 comparable to channel capacity in information theory (Schneider 2006), as the upper bound of  
312 the rate of respiration measured in defined coupling and electron transfer-pathway (ET-  
313 pathway) control states. To provide a diagnostic reference for respiratory capacities of core  
314 energy metabolism, the capacity of *oxidative phosphorylation*, OXPHOS, is measured at  
315 kinetically-saturating concentrations of ADP and inorganic phosphate,  $P_i$ . The *oxidative* ET-  
316 capacity reveals the limitation of OXPHOS-capacity mediated by the *phosphorylation-*  
317 *pathway*. The ET- and phosphorylation-pathways comprise coupled segments of the OXPHOS-  
318 pathway. ET-capacity is measured as noncoupled respiration by application of *external*  
319 *uncouplers*. The contribution of *intrinsically uncoupled* oxygen consumption is most easily  
320 studied in the absence of ADP, *i.e.* by not stimulating phosphorylation, or by inhibition of the  
321 phosphorylation-pathway. The corresponding states are collectively classified as LEAK-states,  
322 when oxygen consumption compensates mainly for the proton leak (**Table 1**). Different  
323 coupling states are induced by (1) adding ADP or  $P_i$ , (2) inhibiting the phosphorylation-  
324 pathway, and (3) performing uncoupler titrations, while maintaining a defined ET-pathway  
325 state with constant fuel substrates and ET inhibitors (**Fig. 1**).

326 **Kinetic control:** Coupling control states are established in the study of mitochondrial  
 327 preparations to obtain reference values for various output variables. Physiological conditions *in*  
 328 *vivo* may deviate substantially from these experimentally obtained states. Since kinetically-  
 329 saturating concentrations, *e.g.* of ADP or oxygen, may not apply to physiological intracellular  
 330 conditions, relevant information is obtained in studies of kinetic responses to conditions  
 331 intermediate between the LEAK state at zero [ADP] and the OXPHOS-state at saturating  
 332 [ADP], or of respiratory capacities in the range between kinetically-saturating [O<sub>2</sub>] and anoxia  
 333 (Gnaiger 2001).



334  
 335 **Fig. 1. The oxidative phosphorylation-pathway, OXPHOS-pathway. (A)** Electron transfer, ET,  
 336 coupled to phosphorylation. Multiple convergent ET-pathways are shown from NADH and succinate;  
 337 additional arrows indicate electron entry through electron transferring flavoprotein, glycerophosphate  
 338 dehydrogenase, dihydro-orotate dehydrogenase, choline dehydrogenase, and sulfide-ubiquinone  
 339 oxidoreductase. The branched pathway of oxygen consumption by alternative quinol oxidase (AOX) is

340 indicated by the dotted arrow. The  $H^+_{out}/O_2$  ratio is the outward proton flux from the matrix space divided  
 341 by catabolic  $O_2$  flux in the NADH-pathway. The  $H^+_{in}/P_{\gg}$  ratio is the inward proton flux from the inter-  
 342 membrane space divided by the flux of phosphorylation of ADP to ATP. Due to proton leak and slip  
 343 these are not fixed stoichiometries. (B) Phosphorylation-pathway catalyzed by the  $F_1F_0$  ATP synthase,  
 344 adenine nucleotide translocase, and inorganic phosphate transporter. The  $H^+_{in}/P_{\gg}$  stoichiometry is the  
 345 sum of the coupling stoichiometry in the ATP synthase reaction (-2.7  $H^+$  from the intermembrane space,  
 346 2.7  $H^+$  to the matrix) and the proton balance in the translocation of  $ADP^{2-}$ ,  $ATP^{3-}$  and  $P_i^{2-}$ . See Eqs. 3  
 347 and 4 for further explanation. Modified from (A) Lemieux *et al.* (2017) and (B) Gnaiger (2014).  
 348



349  
 350 **Fig. 2. The proton circuit and coupling in oxidative phosphorylation (OXPHOS).** Oxygen flux,  $J_{O_2,k}$ ,  
 351 through the catabolic electron transfer-pathway  $k$  is coupled to flux through the phosphorylation-pathway  
 352 of ADP to ATP,  $J_{P_{\gg}}$ , by the proton pumps of the ET-pathway, pushing the outward proton flux,  $J_{H^+,out}$ ,  
 353 and generating the output protonmotive force,  $F_{H^+,out}$ . ATP synthase is coupled to inward proton flux,  
 354  $J_{H^+,in}$ , to phosphorylate  $ADP+P_i$  to ATP, driven by the input protonmotive force,  $F_{H^+,in} = -F_{H^+,out}$ .  $2[H]$   
 355 indicates the reduced hydrogen equivalents of fuel substrates that provide the chemical input force,  $F_{O_2,k}$   
 356 [ $\text{kJ/mol } O_2$ ], of the catabolic reaction  $k$  with oxygen (Gibbs energy of reaction per mole  $O_2$  consumed in  
 357 reaction  $k$ ), typically in the range of -460 to -480  $\text{kJ/mol}$ . The output force is given by the phosphorylation  
 358 potential difference (ADP phosphorylated to ATP),  $F_{P_{\gg}}$ , which varies *in vivo* ranging from about 48 to 62  
 359  $\text{kJ/mol}$  under physiological conditions (Gnaiger 1993a). Fluxes,  $J_B$ , and forces,  $F_B$ , are expressed in  
 360 either chemical units, [ $\text{mol}\cdot\text{s}^{-1}\cdot\text{m}^{-3}$ ] and [ $\text{J}\cdot\text{mol}^{-1}$ ] respectively, or electrical units, [ $\text{C}\cdot\text{s}^{-1}\cdot\text{m}^{-3}$ ] and [ $\text{J}\cdot\text{C}^{-1}$ ]

361 respectively, per volume,  $V$  [m<sup>3</sup>], of the system. The system defined by the boundaries shown as a full  
 362 black line is not a black box, but is analysed as a compartmental system. The negative compartment  
 363 (<sup>-</sup>Compartment, enclosed by the dotted line) is the matrix space, separated from the positive  
 364 compartment (<sup>+</sup>Compartment) by the mtIM. ADP+P<sub>i</sub> and ATP are the substrate- and product-  
 365 compartments (scalar ADP and ATP compartments, <sup>D</sup>Comp. and <sup>T</sup>Comp.), respectively. Chemical  
 366 potentials of all substrates and products involved in the scalar reactions are measured in the  
 367 <sup>+</sup>Compartment for calculation of the scalar forces  $F_{O_2,k}$  and  $F_{P\gg} = -F_{\ll P}$  (**Box 2**). Modified from Gnaiger  
 368 (2014).

369

370 **Phosphorylation, P $\gg$ :** *Phosphorylation* in the context of OXPHOS is defined as  
 371 phosphorylation of ADP to ATP. On the other hand, the term phosphorylation is used generally  
 372 in many different contexts, *e.g.* protein phosphorylation. This justifies consideration of a  
 373 symbol more discriminating and specific than P as used in the P/O ratio (phosphate to atomic  
 374 oxygen ratio;  $O = 0.5 O_2$ ), where P indicates phosphorylation of ADP to ATP or GDP to GTP.  
 375 We propose the symbol P $\gg$  for the endergonic direction of phosphorylation ADP $\rightarrow$ ATP, and  
 376 likewise the symbol  $\ll P$  for the corresponding exergonic hydrolysis ATP $\rightarrow$ ADP (**Fig. 2; Box**  
 377 **3**). ATP synthase is the proton pump of the phosphorylation-pathway (**Fig. 1B**). P $\gg$  may also  
 378 involve substrate-level phosphorylation as part of the tricarboxylic acid cycle (succinyl-CoA  
 379 ligase) and phosphorylation of ADP catalyzed by phosphoenolpyruvate carboxykinase,  
 380 adenylate kinase, creatine kinase, hexokinase and nucleoside diphosphate kinase (NDPK).  
 381 Kinase cycles are involved in intracellular energy transfer and signal transduction for regulation  
 382 of energy flux. In isolated mammalian mitochondria ATP production catalyzed by adenylate  
 383 kinase,  $2ADP \leftrightarrow ATP + AMP$ , proceeds without fuel substrates in the presence of ADP  
 384 (Komlódi and Tretter 2017).  $J_{P\gg}/J_{O_2,k}$  (P $\gg$ /O<sub>2</sub>) is two times the 'P/O' ratio of classical  
 385 bioenergetics. The effective P $\gg$ /O<sub>2</sub> ratio is diminished by: (1) the proton leak across the mtIM  
 386 from low pH in the <sup>+</sup>Compartment to high pH in the <sup>-</sup>Compartment; (2) cycling of other cations;

387 (3) proton slip in the proton pumps when a proton effectively is not pumped; and (4) electron  
 388 leak in the univalent reduction of oxygen ( $O_2$ ; dioxygen) to superoxide anion radical ( $O_2^{\bullet-}$ ).

389

390 **Table 1. Coupling states and residual oxygen consumption in mitochondrial**  
 391 **preparations in relation to respiration- and phosphorylation-rate,  $J_{O_2,k}$  and  $J_{P_{\gg}}$ ,**  
 392 **and protonmotive force,  $F_{H^+,out}$ .** Coupling states are established at kinetically-  
 393 saturating concentrations of fuel substrates and  $O_2$ .

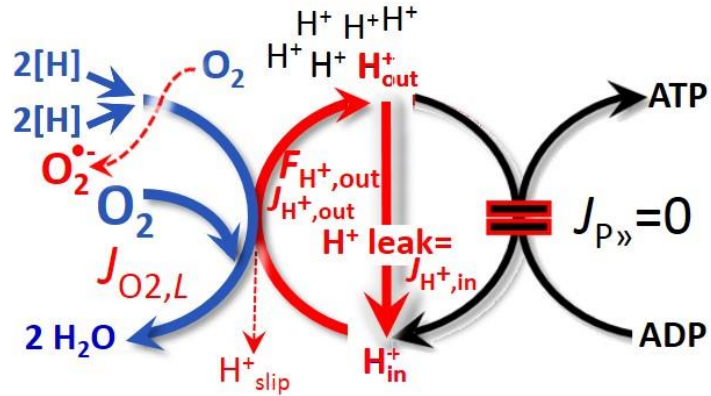
State	$J_{O_2,k}$	$J_{P_{\gg}}$	$F_{H^+,out}$	Inducing factors	Limiting factors
LEAK	$L$ ; low proton leak-dependent respiration	0	max.	Proton leak, slip, and cation cycling	$J_{P_{\gg}} = 0$ : (1) without ADP, $L_N$ ; (2) max. ATP/ADP ratio, $L_T$ ; or (3) inhibition of the phosphorylation-pathway, $L_{Omy}$
OXPHOS	$P$ ; high ADP-stimulated respiration	max.	high	Kinetically-saturating [ADP] and $[P_i]$	$J_{P_{\gg}}$ by phosphorylation-pathway; or $J_{O_2,k}$ by ET-capacity
ET	$E$ ; max. noncoupled respiration	0	low	Optimal external uncoupler concentration for max. oxygen flux	$J_{O_2,k}$ by ET-capacity
ROX	$R_{ox}$ ; min. residual $O_2$ consumption	0	0	$J_{O_2,R_{ox}}$ in non-ET-pathway oxidation reactions	Full inhibition of ET-pathway or absence of fuel substrates

394

395



396 **LEAK-state (Fig. 3):** The  
 397 LEAK-state is defined as a state  
 398 of mitochondrial respiration  
 399 when  $O_2$  flux mainly  
 400 compensates for the proton leak  
 401 in the absence of ATP synthesis,



**Fig. 3. LEAK-state:** Phosphorylation is arrested,  $J_{P \gg} = 0$ , and oxygen flux,  $J_{O_2,L}$ , is controlled mainly by the proton leak, which equals  $J_{H^+,in}$ , at maximum protonmotive force,  $F_{H^+,out}$  (See also Fig. 2).

402 at kinetically-saturating  
 403 concentrations of  $O_2$  and  
 404 respiratory substrates. LEAK-  
 405 respiration is measured to obtain  
 406 an indirect estimate of *intrinsic uncoupling* without addition of any experimental uncoupler: (1)  
 407 in the absence of adenylates; (2) after depletion of ADP at maximum ATP/ADP ratio; or (3)  
 408 after inhibition of the phosphorylation-pathway by inhibitors of ATP synthase, such as  
 409 oligomycin, or adenine nucleotide translocase, such as carboxyatractyloside.

410

411 **Table 2. Distinction of terms related to coupling.**

Term	Respiration	$P \gg / O_2$	Note
Fully coupled	$P - L$	max.	OXPPOS-capacity corrected for LEAK-respiration ( <b>Fig. 6</b> )
Well-coupled	$P$	High	Phosphorylating respiration with a variable intrinsic LEAK component ( <b>Fig. 4</b> )
Loosely coupled	up to $E$	Low	Inducibly uncoupled by UCPI or $Ca^{2+}$ cycling
Dyscoupled	$P$	Low	Pathologically, toxicologically, environmentally increased uncoupling, mitochondrial dysfunction
Uncoupled and decoupled	$L$	0	Non-phosphorylating intrinsic LEAK-respiration without added protonophore ( <b>Fig. 3</b> )
Noncoupled	$E$	0	Non-phosphorylating respiration stimulated to maximum flux at optimum exogenous uncoupler concentration ( <b>Fig. 5</b> )

412



413       **Proton leak:** Proton leak is the *uncoupled* process in which protons are translocated  
414 across the mtIM in the dissipative direction of the downhill protonmotive force without  
415 coupling to phosphorylation (**Fig. 3**). The proton leak flux depends on the protonmotive force,  
416 is a property of the mtIM, may be enhanced due to possible contaminations by free fatty acids,  
417 and is physiologically controlled. In particular, inducible uncoupling mediated by uncoupling  
418 protein 1 (UCP1) is physiologically controlled, *e.g.*, in brown adipose tissue. UCP1 is a proton  
419 channel of the mtIM facilitating the conductance of protons across the mtIM (Klingenberg  
420 2017). As a consequence of this effective short-circuit, the protonmotive force diminishes,  
421 resulting in stimulation of electron transfer to oxygen and heat dissipation without  
422 phosphorylation of ADP. Mitochondrial injuries may lead to *dyscoupling* as a pathological or  
423 toxicological cause of *uncoupled* respiration, *e.g.*, as a consequence of opening the permeability  
424 transition pore. Dyscoupled respiration is distinguished from the experimentally induced  
425 *noncoupled* respiration in the ET-state. Under physiological conditions, the proton leak is the  
426 dominant contributor to the overall leak current (Dufour *et al.* 1996).

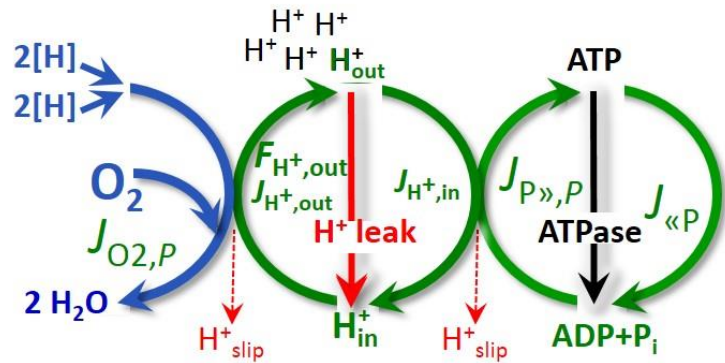
427       **Proton slip:** Proton slip is the *decoupled* process in which protons are only partially  
428 translocated by a proton pump of the ET-pathways and slip back to the original compartment  
429 (Dufour *et al.* 1996). Proton slip can also happen in association with the ATP-synthase, in which  
430 case the proton slips downhill across the membrane to the matrix without contributing to ATP  
431 synthesis. In each case, proton slip is a property of the proton pump and increases with the  
432 turnover rate of the pump.

433       **Cation cycling:** Proton leak is a leak current of protons. There can be other cation  
434 contributors to leak current including calcium and probably magnesium. Calcium current is  
435 balanced by mitochondrial Na/Ca exchange, which is balanced by Na/H exchange or K/H  
436 exchange. This is another effective uncoupling mechanism different from proton leak and slip.

437 Small differences of terms, *e.g.*, uncoupled, noncoupled, are easily overlooked and may  
 438 be erroneously perceived as identical. Even with an attempt at rigorous definition, the common  
 439 use of such terms may remain vague (Table 2).

440 **OXPHOS-state** (Fig. 4):

441 The OXPHOS-state is defined as  
 442 the respiratory state with  
 443 kinetically-saturating  
 444 concentrations of O<sub>2</sub>, respiratory  
 445 and phosphorylation substrates,  
 446 and absence of exogenous  
 447 uncoupler, which provides an  
 448 estimate of the maximal  
 449 respiratory capacity in the



450 **Fig. 4. OXPHOS-state:** Phosphorylation,  $J_{P \gg}$ , is stimulated  
 451 by kinetically-saturating [ADP] and inorganic phosphate,  
 452 [P<sub>i</sub>], and is supported by a high protonmotive force,  $F_{H^+,out}$ .  
 453 O<sub>2</sub> flux,  $J_{O_2,P}$ , is well-coupled at a P<sub>i</sub>/O<sub>2</sub> ratio of  $J_{P \gg, P}/J_{O_2,P}$ .  
 454 (See also Fig. 2).

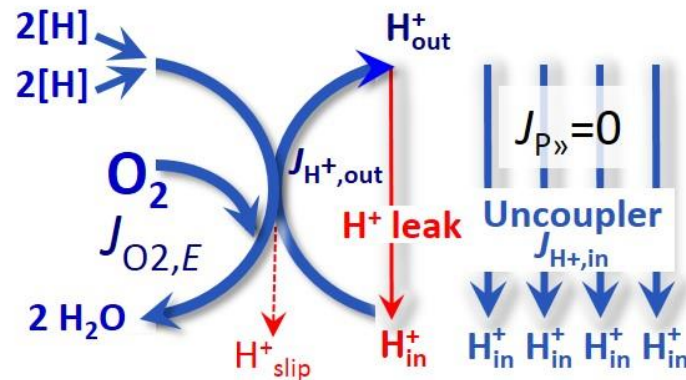
450 OXPHOS-state for any given ET-pathway state. Respiratory capacities at kinetically-saturating  
 451 substrate concentrations provide reference values or upper limits of performance, aiming at the  
 452 generation of data sets for comparative purposes. Any effects of substrate kinetics are thus  
 453 separated from reporting actual mitochondrial capacity for oxidation during well-coupled  
 454 respiration, against which physiological activities can be evaluated.

455 As discussed previously, 0.2 mM ADP does not fully saturate flux in isolated  
 456 mitochondria (Gnaiger 2001; Puchowicz *et al.* 2004); greater ADP concentration is required,  
 457 particularly in permeabilized muscle fibres and cardiomyocytes, to overcome limitations by  
 458 intracellular diffusion and by the reduced conductance of the mitochondrial outer membrane,  
 459 mtOM (Jepihhina *et al.* 2011, Illaste *et al.* 2012, Simson *et al.* 2016) either through interaction  
 460 with tubulin (Rostovtseva *et al.* 2008) or other intracellular structures (Birkedal *et al.* 2014). In  
 461 permeabilized muscle fibre bundles of high respiratory capacity, the apparent  $K_m$  for ADP  
 462 increases up to 0.5 mM (Saks *et al.* 1998), indicating that >90% saturation is reached only at

463 >5 mM ADP. Similar ADP concentrations are also required for accurate determination of  
 464 OXPHOS-capacity in human clinical cancer samples and permeabilized cells (Klepinin *et al.*  
 465 2016; Koit *et al.* 2017). Whereas 2.5 to 5 mM ADP is sufficient to obtain the actual OXPHOS-  
 466 capacity in many types of permeabilized cell and tissue preparations, experimental validation  
 467 is required in each specific case.

### Electron transfer-state

468 (Fig. 5): The ET-state is defined  
 469 as the *noncoupled* state with  
 470 kinetically-saturating  
 471 concentrations of O<sub>2</sub>, respiratory  
 472 substrate and optimum  
 473 exogenous uncoupler  
 474 concentration for maximum O<sub>2</sub>  
 475 flux, as an estimate of oxidative



476 flux, as an estimate of oxidative  
 477 ET-capacity. Inhibition of respiration is observed at higher than optimum uncoupler  
 478 concentrations. As a consequence of the nearly collapsed protonmotive force, the driving force  
 479 is insufficient for phosphorylation and  $J_{P} = 0$ .  
**Fig. 5. ET-state:** Noncoupled respiration,  $J_{O_2,E}$ , is maximum  
 at optimum exogenous uncoupler concentration and  
 phosphorylation is zero,  $J_{P} = 0$  (See also Fig. 2).

477 ET-capacity. Inhibition of respiration is observed at higher than optimum uncoupler  
 478 concentrations. As a consequence of the nearly collapsed protonmotive force, the driving force  
 479 is insufficient for phosphorylation and  $J_{P} = 0$ .

480 Besides the three fundamental coupling states of mitochondrial preparations, the  
 481 following respiratory state also is relevant to assess respiratory function:

482 **ROX:** Residual oxygen consumption (ROX) is defined as O<sub>2</sub> consumption due to  
 483 oxidative side reactions remaining after inhibition of ET with rotenone, malonic acid and  
 484 antimycin A. Cyanide and azide not only inhibit CIV but several peroxidases which might be  
 485 involved in ROX. ROX is not a coupling state but represents a baseline that is used to correct  
 486 mitochondrial respiration in defined coupling states. ROX is not necessarily equivalent to non-  
 487 mitochondrial respiration, considering oxygen-consuming reactions in mitochondria not related  
 488 to ET, such as oxygen consumption in reactions catalyzed by monoamine oxidases (type A and

489 B), monooxygenases (cytochrome P450 monooxygenases), dioxygenase (sulfur dioxygenase  
 490 and trimethyllysine dioxygenase), several hydroxylases, and more. Mitochondrial preparations,  
 491 especially those obtained from liver, are contaminated by peroxisomes. This fact makes the  
 492 exact determination of mitochondrial oxygen consumption and mitochondria-associated  
 493 generation of reactive oxygen species complicated (Schönfeld *et al.* 2009). The dependence of  
 494 ROX-linked oxygen consumption needs to be studied in detail with respect to non-ET enzyme  
 495 activities, availability of specific substrates, oxygen concentration, and electron leakage leading  
 496 to the formation of reactive oxygen species.

497

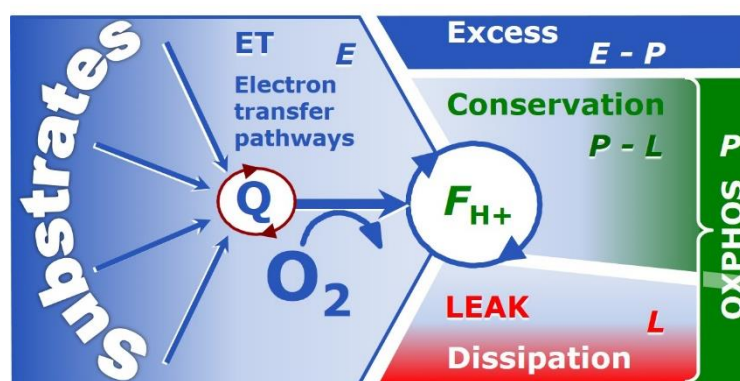
## 498 2.2. Coupling states and respiratory rates

499 It is important to distinguish metabolic pathways from metabolic states and the  
 500 corresponding metabolic rates; for example: ET-pathways (Fig. 6), ET-state (Fig. 5), and ET-  
 501 capacity,  $E$ , respectively (Table 1). The protonmotive force is *high* in the OXPHOS-state when  
 502 it drives phosphorylation, *maximum* in the LEAK-state of coupled mitochondria, driven by  
 503 LEAK-respiration at a minimum back flux of protons to the matrix side, and *very low* in the  
 504 ET-state when uncouplers short-circuit the proton cycle (Table 1).

505

506 **Fig. 6. Four-compartment model**  
 507 **of oxidative phosphorylation.**

508 Respiratory states (ET, OXPHOS,  
 509 LEAK) and corresponding rates ( $E$ ,  
 510  $P$ ,  $L$ ) are connected by the  
 511 protonmotive force,  $F_{H+,out}$ . Electron  
 512 transfer-capacity,  $E$ , is partitioned



513 into (1) dissipative LEAK-respiration,  $L$ , when the capacity to perform work is irreversibly lost, (2) net  
 514 OXPHOS-capacity,  $P-L$ , with partial conservation of the capacity to perform work, and (3) the excess  
 515 capacity,  $E-P$ . Modified from Gnaiger (2014).

516

517 The three coupling states, ET, LEAK and OXPHOS, are presented in a schematic context  
518 with the corresponding respiratory rates, abbreviated as  $E$ ,  $L$  and  $P$ , respectively (Fig. 6). This  
519 clarifies that  $E$  may exceed or be equal to  $P$ , but  $E$  cannot theoretically be lower than  $P$ .  $E < P$   
520 must be discounted as an artefact, which may be caused experimentally by: (1) loss of oxidative  
521 capacity during the time course of the respirometric assay, since  $E$  is measured subsequently to  
522  $P$ ; (2) using insufficient uncoupler concentrations; (3) using high uncoupler concentrations which  
523 inhibit ET (Gnaiger 2008); (4) high oligomycin concentrations applied for measurement of  $L$   
524 before titrations of uncoupler, when oligomycin exerts an inhibitory effect on  $E$ . On the other  
525 hand, the excess ET-capacity is overestimated if non-saturating  $[P_i]$  or  $[ADP]$  are used (see  
526 State 3 in the next section).

527  $E > P$  is observed in many types of mitochondria, varying between species, tissues and  
528 cell types. It is the excess ET-capacity pushing the phosphorylation-flux (Fig. 1B) to the limit  
529 of its *capacity of utilizing* the protonmotive force. Within any type of mitochondria, the  
530 magnitude of  $E > P$  depends on (1) the pathway control state with single or multiple electron  
531 input into the Q-junction and involvement of three or fewer coupling sites determining the  
532  $H^+_{out}/O_2$  *coupling stoichiometry* (Fig. 1A); and (2) the *biochemical coupling efficiency*  
533 expressed as  $(E-L)/E$ , since an increase of  $L$  causes  $P$  to increase towards the limit of  $E$ . The  
534 *excess E-P capacity*,  $E-P$ , therefore, provides a sensitive diagnostic indicator of specific injuries  
535 of the phosphorylation-pathway, under conditions when  $E$  remains constant but  $P$  declines  
536 relative to controls (Fig. 6). Substrate cocktails supporting simultaneous convergent electron  
537 transfer to the Q-junction for reconstitution of tricarboxylic acid cycle (TCA cycle) function  
538 establish pathway control states with high ET-capacity, and consequently increase the  
539 sensitivity of the  $E-P$  assay.

540 When subtracting  $L$  from  $P$ , the dissipative LEAK component in the OXPHOS-state may  
541 be overestimated. This can be avoided by measuring LEAK-respiration in a state when the  
542 protonmotive force is adjusted to its slightly lower value in the OXPHOS-state, *e.g.*, by titration

543 of an ET inhibitor. Any turnover-dependent components of proton leak and slip, however, are  
 544 underestimated under these conditions (Garlid *et al.* 1993). In general, it is inappropriate to use  
 545 the term *ATP production* or *ATP turnover* for the difference of oxygen consumption measured  
 546 in states *P* and *L*. The difference *P-L* is the upper limit of the part of OXPHOS-capacity that is  
 547 freely available for ATP production (corrected for LEAK-respiration) and is fully coupled to  
 548 phosphorylation with a maximum mechanistic stoichiometry (**Fig. 6**).

549

### 550 2.3. Classical terminology for isolated mitochondria

551 *‘When a code is familiar enough, it ceases appearing like a code; one forgets that*  
 552 *there is a decoding mechanism. The message is identical with its meaning’*  
 553 (Hofstadter 1979).

554 Chance and Williams (1955; 1956) introduced five classical states of mitochondrial respiration  
 555 and cytochrome redox states. **Table 3** shows a protocol with isolated mitochondria in a closed  
 556 respirometric chamber, defining a sequence of respiratory states.

557 **Table 3. Metabolic states of mitochondria (Chance and**  
 558 **Williams, 1956; Table V).**  
 559

State	[O <sub>2</sub> ]	ADP level	Substrate level	Respiration rate	Rate-limiting substance
1	>0	low	low	slow	ADP
2	>0	high	~0	slow	substrate
3	>0	high	high	fast	respiratory chain
4	>0	low	high	slow	ADP
5	0	high	high	0	oxygen

560

561 **State 1** is obtained after addition of isolated mitochondria to air-saturated  
 562 isoosmotic/isotonic respiration medium containing inorganic phosphate, but no fuel substrates  
 563 and no adenylates, *i.e.*, AMP, ADP, ATP.

564 **State 2** is induced by addition of a high concentration of ADP (typically 100 to 300  $\mu$ M),  
 565 which stimulates respiration transiently on the basis of endogenous fuel substrates and

566 phosphorylates only a small portion of the added ADP. State 2 is then obtained at a low  
567 respiratory activity limited by zero endogenous fuel substrate availability (**Table 3**). If addition  
568 of specific inhibitors of respiratory complexes, such as rotenone, does not cause a further  
569 decline of oxygen consumption, State 2 is equivalent to residual oxygen consumption (See  
570 below). If inhibition is observed, undefined endogenous fuel substrates are a confounding factor  
571 of pathway control by externally added substrates and inhibitors. In contrast to the original  
572 protocol, an alternative sequence of titration steps is frequently applied, in which the alternative  
573 State 2 has an entirely different meaning, when this second state is induced by addition of fuel  
574 substrate without ADP (LEAK-state; in contrast to State 2 defined in **Table 2** as a ROX state),  
575 followed by addition of ADP.

576 **State 3** is the state stimulated by addition of fuel substrates while the ADP concentration  
577 is still high (**Table 3**) and supports coupled energy transformation through oxidative  
578 phosphorylation. 'High ADP' is a concentration of ADP specifically selected to allow the  
579 measurement of State 3 to State 4 transitions of isolated mitochondria in a closed respirometric  
580 chamber. Repeated ADP titration re-establishes State 3 at 'high ADP'. Starting at oxygen  
581 concentrations near air-saturation (ca. 200  $\mu\text{M}$   $\text{O}_2$  at sea level and 37 °C), the total ADP  
582 concentration added must be low enough (typically 100 to 300  $\mu\text{M}$ ) to allow phosphorylation  
583 to ATP at a coupled oxygen consumption that does not lead to oxygen depletion during the  
584 transition to State 4. In contrast, kinetically-saturating ADP concentrations usually are an order  
585 of magnitude higher than 'high ADP', e.g. 2.5 mM in isolated mitochondria. The abbreviation  
586 State 3u is frequently used in bioenergetics, to indicate the state of respiration after titration of  
587 an uncoupler, without sufficient emphasis on the fundamental difference between OXPHOS-  
588 capacity (*well-coupled* with an *endogenous* uncoupled component) and ET-capacity  
589 (*noncoupled*).

590 **State 4** is a LEAK-state that is obtained only if the mitochondrial preparation is intact  
591 and well-coupled. Depletion of ADP by phosphorylation to ATP leads to a decline in oxygen



592 consumption in the transition from State 3 to State 4. Under these conditions, a maximum  
 593 protonmotive force and high ATP/ADP ratio are maintained, and the  $P_{\gg}/O_2$  ratio can be  
 594 calculated. State 4 respiration,  $L_T$  (**Table 1**), reflects intrinsic proton leak and intrinsic ATP  
 595 hydrolysis activity. Oxygen consumption in State 4 is an overestimation of LEAK-respiration  
 596 if the contaminating ATP hydrolysis activity recycles some ATP to ADP,  $J_{\ll P}$ , which stimulates  
 597 respiration coupled to phosphorylation,  $J_{P\gg} > 0$ . This can be tested by inhibition of the  
 598 phosphorylation-pathway using oligomycin, ensuring that  $J_{P\gg} = 0$  (State 4o). Alternatively,  
 599 sequential ADP titrations re-establish State 3, followed by State 3 to State 4 transitions while  
 600 sufficient oxygen is available. However, anoxia may be reached before exhaustion of ADP  
 601 (State 5).

602 **State 5** is the state after exhaustion of oxygen in a closed respirometric chamber.  
 603 Diffusion of oxygen from the surroundings into the aqueous solution may be a confounding  
 604 factor preventing complete anoxia (Gnaiger 2001). Chance and Williams (1955) provide an  
 605 alternative definition of State 5, which gives it the meaning of ROX: ‘State 5 may be obtained  
 606 by antimycin A treatment or by anaerobiosis’.

607 In **Table 3**, only States 3 and 4 (and ‘State 2’ in the alternative protocol without ADP;  
 608 not included in the table) are coupling control states, with the restriction that  $O_2$  flux in State 3  
 609 may be limited kinetically by non-saturating ADP concentrations (**Table 1**).

610

### 611 **3. The protonmotive force and proton flux**

#### 612 *3.1. Electric and chemical partial forces versus electrical and chemical units*

613 The protonmotive force across the mtIM (Mitchell and Moyle 1967) was introduced most  
 614 beautifully in the *Grey Book 1966* (see Mitchell 2011),

$$615 \quad \Delta p_{H^+} = \Delta \Psi + \Delta \mu_{H^+}/F \quad (\text{Eq. 1})$$

616 The protonmotive force consists of two partial forces: (I) The electrical part,  $\Delta \Psi$ , is the  
 617 difference of charge (electric potential difference), is not specific for  $H^+$ , and can, therefore, be



618 measured by the distribution of other cations between the positive and negative compartment  
 619 (**Fig. 2**). (2) The chemical part,  $\Delta\mu_{H^+}$ , is the chemical potential difference in  $H^+$ , is proportional  
 620 to the pH difference, and incorporates the Faraday constant (**Table 4**).

621  
 622 **Table 4. Protonmotive force and flux matrix.** Columns: The protonmotive force is  
 623 the sum of *partial isomorphic forces*,  $F_{el}$  and  $F_{H^+,d}$ . Rows: Electrical and chemical units  
 624 (isomorphic format  $e$  and  $n$ ). The Faraday constant,  $F$ , converts protonmotive force  
 625 and flux from *format e* to  $n$ . In contrast to force (state), the conjugated flux (rate) cannot  
 626 be partitioned.  
 627

State	Force		electric	+ chem.	Unit	Notes
Protonmotive force, $e$	$\Delta p_{H^+}$	=	$\Delta\Psi$	+ $\Delta\mu_{H^+}/F$	$J\cdot C^{-1}$	$1e$
Chemiosmotic potential, $n$	$\Delta\tilde{\mu}_{H^+}$	=	$\Delta\Psi\cdot F$	+ $\Delta\mu_{H^+}$	$J\cdot mol^{-1}$	$1n$
State	Isomorphic force		$F_{H^+,out/i}$	$e_{out}$	+ $H^+_{out,d}$	
Electric charge, $e$	$F_{H^+,out/e}$	=	$F_{el,out/e}$	+ $F_{H^+,out,d/e}$	$J\cdot C^{-1}$	$2e$
Amount of substance, $n$	$F_{H^+,out/n}$	=	$F_{el,out/n}$	+ $F_{H^+,out,d/n}$	$J\cdot mol^{-1}$	$2n$
Rate	Isomorphic flux		$J_{H^+,out/i}$	$e$	or	$n$
Electric charge, $e$	$J_{H^+,out/e}$		$J_{H^+,out/e}$			$C\cdot s^{-1}\cdot m^{-3}$ $3e$
Amount of substance, $n$	$J_{H^+,out/n}$				$J_{H^+,out/n}$	$mol\cdot s^{-1}\cdot m^{-3}$ $3n$

628  
 629 1: The Faraday constant,  $F$ , is the product of elementary charge ( $e = 1.602177\cdot 10^{-19}\cdot C$ ) and the  
 630 Avogadro (Loschmidt) constant ( $N_A = 6.022136\cdot 10^{23}\cdot mol^{-1}$ ),  $F = eN_A = 96,485.3 C/mol$ .  $\Delta\tilde{\mu}_{H^+}$  is the  
 631 chemiosmotic potential difference.  $1e$  and  $1n$  are the classical representations of  $2e$  and  $2n$ .  
 632 2: The protonmotive force is  $F_{H^+,out}$ , expressed either in isomorphic format  $e$  or  $n$ .  $F_{el/e} \equiv \Delta\Psi$  is the partial  
 633 protonmotive force ( $e$ ) acting generally on charged motive molecules (*i.e.* ions that are displaceable  
 634 across the mtIM). In contrast,  $F_{H^+,d/n} \equiv \Delta\mu_{H^+}$  is the partial protonmotive force specific for proton  
 635 displacement ( $H^+_d$ ). The sign of the force is negative for exergonic transformations in which exergy  
 636 is lost or dissipated, and positive for endergonic transformations which conserve exergy from a  
 637 coupled exergonic process (**Box 3**).  
 638 3: The sign of the flux depends on the definition of the compartmental direction of the translocation (**Fig.**  
 639 **2**). Flux x force =  $J_{H^+,out/e}\cdot F_{H^+,out/e} = J_{H^+,out/n}\cdot F_{H^+,out/n}$  = volume-specific power [ $J\cdot s^{-1}\cdot m^{-3} = W\cdot m^{-3}$ ].

640

641 **Faraday constant**,  $F = eN_A$  [C/mol] (**Table 4**), enables the conversion between  
 642 protonmotive force,  $F_{H+,out/e} \equiv \Delta p_{H+}$  [J/C], expressed per *motive charge*,  $e$  [C], and protonmotive  
 643 force or electrochemical potential difference,  $F_{H+,out/n} \equiv \Delta \tilde{\mu}_{H+} = \Delta p_{H+} \cdot F$  [J/mol], expressed per  
 644 *motive amount of protons*,  $n$  [mol]. Proton charge,  $e$ , and amount of substance,  $n$ , define the  
 645 units for the isomorphic formats. Taken together,  $F$  converts protonmotive force and flux from  
 646 isomorphic format  $e$  to  $n$  (Eq. 2; see also **Table 4**, Note 2),

$$647 \quad F_{H+,out/n} = F_{H+,out/e} \cdot eN_A \quad (\text{Eq. 2.1})$$

$$648 \quad J_{H+,out/n} = J_{H+,out/e} / (eN_A) \quad (\text{Eq. 2.2})$$

649 In each format, the protonmotive force is expressed as the sum of two partial forces. The  
 650 concept expressed by the complex symbols in Eq. 1 can be explained and visualized more easily  
 651 by *partial isomorphic forces* as the components of the protonmotive force:

652 **Electrical part of the protonmotive force:** (1) Isomorph  $e$ :  $F_{el/e} \equiv \Delta \Psi$  is the electrical  
 653 part of the protonmotive force expressed in units joule per coulomb, *i.e.* volt [ $V = J/C$ ].  $F_{el/e}$  is  
 654 defined as partial Gibbs energy change per *motive elementary charge*,  $e$  [C], not specific for  
 655 proton charge (**Table 4**, Note 2e). (2) Isomorph  $n$ :  $F_{el/n} \equiv \Delta \Psi \cdot F$  is the electric force expressed  
 656 in units joule per mole [J/mol], defined as partial Gibbs energy change per *motive amount of*  
 657 *charge*,  $n$  [mol], not specific for proton charge (**Table 4**, Note 2n).

658 **Chemical part of the protonmotive force:** (1) Isomorph  $n$ :  $F_{d,H+/n} \equiv \Delta \mu_{H+}$  is the chemical  
 659 part (diffusion, displacement of  $H^+$ ) of the protonmotive force expressed in units joule per mole  
 660 [J/mol].  $F_{d,H+/n}$  is defined as partial Gibbs energy change per *motive amount of protons*,  $n$  [mol]  
 661 (**Table 4**, Note 2n). (2) Isomorph  $e$ :  $F_{d,H+/e} \equiv \Delta \mu_{H+} / F$  is the chemical force expressed in units  
 662 joule per coulomb [V], defined as partial Gibbs energy change per *motive amount of protons*  
 663 *expressed in units of electric charge*,  $e$  [C], but specific for proton charge (**Table 4**, Note 2e).

664 Protonmotive means that there is a potential for the movement of protons, and force is a  
 665 measure of the potential for motion. Motion is relative and not absolute (Principle of Galilean

666 Relativity); likewise there is no absolute potential, but (isomorphic) forces are potential  
667 differences. An electric partial force expressed in the format of electric charge,  $F_{el/e}$ , of -0.2 V  
668 (**Table 5**, Note 5e) is equivalent to force in the format of amount,  $F_{el,H+/n}$ , of  $19 \text{ kJ}\cdot\text{mol}^{-1} \text{ H}^+_{\text{out}}$   
669 (Note 5n). For a  $\Delta\text{pH}$  of 1 unit, the chemical partial force in the format of amount,  $F_{d,H+/n}$ ,  
670 changes by  $5.9 \text{ kJ}\cdot\text{mol}^{-1}$  (**Table 5**, Note 6n) and chemical force in the format of charge  $F_{d,H+/e}$   
671 changes by 0.06 V (Note 6e). Considering a driving force of  $-470 \text{ kJ}\cdot\text{mol}^{-1} \text{ O}_2$  for oxidation, the  
672 thermodynamic limit of the  $\text{H}^+_{\text{out}}/\text{O}_2$  ratio is reached at a value of  $470/19 = 24$ , compared to a  
673 mechanistic stoichiometry of 20 (**Fig. 1**).

674

### 675 3.2. Definitions

676 **Control and regulation:** The terms metabolic *control* and *regulation* are frequently used  
677 synonymously, but are distinguished in metabolic control analysis: ‘We could understand the  
678 regulation as the mechanism that occurs when a system maintains some variable constant over  
679 time, in spite of fluctuations in external conditions (homeostasis of the internal state). On the  
680 other hand, metabolic control is the power to change the state of the metabolism in response to  
681 an external signal’ (Fell 1997). Respiratory control may be induced by experimental control  
682 signals that *exert* an influence on: (1) ATP demand and ADP phosphorylation-rate; (2) fuel  
683 substrate composition, pathway competition; (3) available amounts of substrates and oxygen,  
684 *e.g.*, starvation and hypoxia; (3) the protonmotive force, redox states, flux-force relationships,  
685 coupling and efficiency; (4)  $\text{Ca}^{2+}$  and other ions including  $\text{H}^+$ ; (5) inhibitors, *e.g.*, nitric oxide  
686 or intermediary metabolites, such as oxaloacetate; (6) signalling pathways and regulatory  
687 proteins, *e.g.* insulin resistance, transcription factor HIF-1 or inhibitory factor 1. *Mechanisms*  
688 of respiratory control and regulation include adjustments of (1) enzyme activities by allosteric  
689 mechanisms and phosphorylation, (2) enzyme content, concentrations of cofactors and  
690 conserved moieties (such as adenylates, nicotinamide adenine dinucleotide [ $\text{NAD}^+/\text{NADH}$ ],  
691 coenzyme Q, cytochrome *c*); (3) metabolic channeling by supercomplexes; and (4)

692 mitochondrial density (enzyme concentrations and membrane area) and morphology (cristae  
693 folding, fission and fusion). (5) Mitochondria are targeted directly by hormones, thereby  
694 affecting their energy metabolism (Lee *et al.* 2013; Gerö and Szabo 2016; Price and Dai 2016;  
695 Moreno *et al.* 2017). Evolutionary or acquired differences in the genetic and epigenetic basis  
696 of mitochondrial function (or dysfunction) between subjects and gene therapy; age; gender,  
697 biological sex, and hormone concentrations; life style including exercise and nutrition; and  
698 environmental issues including thermal, atmospheric, toxicological and pharmacological  
699 factors, exert an influence on all control mechanisms listed above (for reviews, see Brown 1992;  
700 Gnaiger 1993a, 2009; 2014; Paradies *et al.* 2014; Morrow *et al.* 2017).

701       **Respiratory control and response:** Lack of control by a metabolic pathway, *e.g.*  
702 phosphorylation-pathway, does mean that there will be no response to a variable activating it,  
703 *e.g.* [ADP]. However, the reverse is not true as the absence of a response to [ADP] does not  
704 exclude the phosphorylation-pathway from having some degree of control. The degree of  
705 control of a component of the OXPHOS-pathway on an output variable, such as oxygen flux,  
706 will in general be different from the degree of control on other outputs, such as phosphorylation-  
707 flux or proton leak flux (**Box 2**). As such, it is necessary to be specific as to which input and  
708 output are under consideration (Fell 1997). Therefore, the term respiratory control is elaborated  
709 in more detail in the following section.

710       **Respiratory coupling control:** Respiratory control refers to the ability of mitochondria  
711 to adjust oxygen consumption in response to external control signals by engaging various  
712 mechanisms of control and regulation. Respiratory control is monitored in a mitochondrial  
713 preparation under conditions defined as respiratory states. When phosphorylation of ADP to  
714 ATP is stimulated or depressed, an increase or decrease is observed in electron flux linked to  
715 oxygen consumption in respiratory coupling states of intact mitochondria ('controlled states' in  
716 the classical terminology of bioenergetics). Alternatively, coupling of electron transfer with  
717 phosphorylation is disengaged by disruption of the integrity of the mtIM or by uncouplers,

718 functioning like a clutch in a mechanical system. The corresponding coupling control state is  
 719 characterized by high levels of oxygen consumption without control by phosphorylation  
 720 ('uncontrolled state'). Energetic coupling is defined in **Box 4**. Loss of coupling lowers the  
 721 efficiency by intrinsic uncoupling and decoupling, or pathological dyscoupling. Such  
 722 generalized uncoupling is different from switching to mitochondrial pathways that involve  
 723 fewer than three proton pumps ('coupling sites': Complexes CI, CIII and CIV), bypassing CI  
 724 through multiple electron entries into the Q-junction (**Fig. 1**). A bypass of CIII and CIV is  
 725 provided by alternative oxidases, which reduce oxygen without proton translocation.  
 726 Reprogramming of mitochondrial pathways may be considered as a switch of gears (changing  
 727 the stoichiometry) rather than uncoupling (loosening the stoichiometry).

728 **Pathway control states** are obtained in mitochondrial preparations by depletion of  
 729 endogenous substrates and addition to the mitochondrial respiration medium of fuel substrates  
 730 (CHNO) and specific inhibitors, activating selected mitochondrial pathways (**Fig. 1**). Coupling  
 731 control states and pathway control states are complementary, since mitochondrial preparations  
 732 depend on an exogenous supply of pathway-specific fuel substrates and oxygen (Gnaiger 2014).

733

---

734 **Box 2: Metabolic fluxes and flows: vectorial and scalar**

735 In mitochondrial electron transfer (**Fig. 1**), vectorial transmembrane proton flux is coupled  
 736 through the proton pumps CI, CIII and CIV to the catabolic flux of scalar reactions, collectively  
 737 measured as oxygen flux. In **Fig. 2**, the scalar catabolic reaction,  $k$ , of oxygen consumption,  
 738  $J_{O_2,k}$  [ $\text{mol}\cdot\text{s}^{-1}\cdot\text{m}^{-3}$ ], is expressed as oxygen flux per volume,  $V$  [ $\text{m}^3$ ], of the instrumental chamber  
 739 (the system).

740 Fluxes are *vectors*, if they have *spatial* direction in addition to magnitude. A vector flux  
 741 (surface-density of flow) is expressed per unit cross-sectional area,  $A$  [ $\text{m}^2$ ], perpendicular to the  
 742 direction of flux. If *flows*,  $I$ , are defined as extensive quantities of the *system*, as vector or scalar  
 743 flow,  $I$  or  $I$  [ $\text{mol}\cdot\text{s}^{-1}$ ], respectively, then the corresponding vector and scalar *fluxes*,  $J$ , are

744 obtained as  $J = I \cdot A^{-1}$  [ $\text{mol} \cdot \text{s}^{-1} \cdot \text{m}^{-2}$ ] and  $J = I \cdot V^{-1}$  [ $\text{mol} \cdot \text{s}^{-1} \cdot \text{m}^{-3}$ ], respectively, expressing flux as an  
 745 area-specific vector or volume-specific scalar quantity.

746 Vectorial transmembrane proton flux,  $J_{\text{H}^+, \text{out}}$ , is analyzed in a heterogenous  
 747 compartmental system as a quantity with *directional* but not *spatial* information. Translocation  
 748 of protons across the mtIM has a defined direction, either from the negative compartment  
 749 (matrix space; negative or  $\bar{\text{Compartment}}$ ) to the positive compartment (inter-membrane space;  
 750 positive or  $^+\text{Compartment}$ ) or *vice versa* (**Fig. 2**). The arrows defining the direction of the  
 751 translocation between the two compartments may point upwards or downwards, right or left,  
 752 without any implication that these are actual directions in space. The ‘upper’ compartment of  
 753 the  $^+\text{Compartment}$  is neither above nor below the  $\bar{\text{Compartment}}$  in a spatial sense, but can be  
 754 visualized arbitrarily in a figure as the upper compartment (**Fig. 2**). In general, the  
 755 *compartmental direction* of vectorial translocation from the  $\bar{\text{Compartment}}$  to the  
 756  $^+\text{Compartment}$  is defined by assigning the initial and final state as *ergodynamic compartments*,  
 757  $\text{H}^+_{\text{in}} \rightarrow \text{H}^+_{\text{out}}$ , respectively, related to work (erg = work) that must be performed to lift the proton  
 758 from a lower to a higher electrochemical potential or from the lower to the higher ergodynamic  
 759 compartment (Gnaiger 1993b).

760 In direct analogy to *vectorial* translocation, the direction of a *scalar* chemical reaction,  $\text{A}$   
 761  $\rightarrow \text{B}$ , is defined by assigning substrates and products, A and B, as ergodynamic compartments.  
 762  $\text{O}_2$  is defined as a substrate in respiratory  $\text{O}_2$  consumption, which together with the fuel  
 763 substrates comprises the substrate compartment of the catabolic reaction (**Fig. 2**). Volume-  
 764 specific scalar  $\text{O}_2$  flux is coupled (**Box 4**) to vectorial translocation. In order to establish a  
 765 quantitative relation between the coupled fluxes, both  $J_{\text{O}_2, \text{k}}$  and  $J_{\text{H}^+, \text{out}}$  must be expressed in  
 766 identical isomorphic units ( $[\text{mol} \cdot \text{s}^{-1} \cdot \text{m}^{-3}]$  or  $[\text{C} \cdot \text{s}^{-1} \cdot \text{m}^{-3}]$ ), yielding the  $\text{H}^+_{\text{out}}/\text{O}_2$  ratio (**Fig. 1**). The  
 767 *vectorial* proton flux in compartmental translocation has *compartmental direction*,  
 768 distinguished from a *vector* flux with *spatial direction*. Likewise, the corresponding  
 769 protonmotive force is defined as an electrochemical potential *difference* between two

770 compartments, in contrast to a *gradient* across the membrane or a vector force with defined  
 771 spatial direction.

772

---

773 **The steady-state:** Mitochondria represent a thermodynamically open system functioning  
 774 as a biochemical transformation system in non-equilibrium states. State variables (protonmotive  
 775 force; redox states) and metabolic fluxes (*rates*) are measured in defined mitochondrial  
 776 respiratory *states*. Strictly, steady states can be obtained only in open systems, in which changes  
 777 due to *internal* transformations, *e.g.*, O<sub>2</sub> consumption, are instantaneously compensated for by  
 778 *external* fluxes *e.g.*, O<sub>2</sub> supply, such that oxygen concentration does not change in the system  
 779 (Gnaiger 1993b). Mitochondrial respiratory states monitored in closed systems satisfy the  
 780 criteria of pseudo-steady states for limited periods of time, when changes in the system  
 781 (concentrations of O<sub>2</sub>, fuel substrates, ADP, P<sub>i</sub>, H<sup>+</sup>) do not exert significant effects on metabolic  
 782 fluxes (respiration, phosphorylation). Such pseudo-steady states require respiratory media with  
 783 sufficient buffering capacity and kinetically-saturating concentrations of substrates to be  
 784 maintained, and thus depend on the kinetics of the processes under investigation. Proton  
 785 turnover,  $J_{\infty H^+}$ , and ATP turnover,  $J_{\infty P}$ , proceed in the steady-state at constant  $F_{H^+,out}$ , when  $J_{\infty H^+}$   
 786  $= J_{H^+,out} = J_{H^+,in}$ , and at constant  $F_{P\gg}$ , when  $J_{\infty P} = J_{P\gg} = J_{\ll P}$  (**Fig. 2**).

787

---

### 788 **Box 3: Endergonic and exergonic transformations, exergy and dissipation**

789 A chemical reaction, or any transformation, is exergonic if the Gibbs energy change (exergy)  
 790 of the reaction is negative at constant temperature and pressure. The sum of Gibbs energy  
 791 changes of all internal transformations in a system can only be negative, *i.e.* exergy is  
 792 irreversibly dissipated. Endergonic reactions are characterized by positive Gibbs energies of  
 793 reaction and cannot proceed spontaneously in the forward direction as defined. For instance,  
 794 the endergonic reaction P $\gg$  is coupled to exergonic catabolic reactions, such that the total Gibbs  
 795 energy change is negative, *i.e.* exergy must be dissipated for the reaction to proceed (**Fig. 2**).

796 In contrast, energy cannot be lost or produced in any internal process, which is the key  
 797 message of the first law of thermodynamics. Thus mitochondria are the sites of energy  
 798 transformation but not energy production. Open and closed systems can gain energy and exergy  
 799 only by external fluxes, *i.e.* uptake from the environment. Exergy is the potential to perform  
 800 work. In the framework of flux-force relationships (**Box 4**), the *partial* derivative of Gibbs  
 801 energy per advancement of a transformation is an isomorphic force,  $F_{tr}$  (**Table 5**, Note 2). In  
 802 other words, force is equal to exergy/motive unit (in integral form, this definition takes care of  
 803 non-isothermal processes). This formal generalization represents an appreciation of the  
 804 conceptual beauty of Peter Mitchell's innovation of the protonmotive force against the  
 805 background of the established paradigm of the electromotive force (emf) defined at the limit of  
 806 zero current (Cohen *et al.* 2008).

807

808

809 **Table 5. Power, exergy, force, flux, and advancement.**

810

Expression	Symbol	Definition	Unit	Notes
Power, volume-specific	$P_{V,tr}$	$P_{V,tr} = J_{tr} \cdot F_{tr} = \hat{\partial}_{tr}G \cdot \partial t^{-1}$	$W = J \cdot s^{-1} \cdot m^{-3}$	1
Force, isomorphic	$F_{tr}$	$F_{tr} = \hat{\partial}_{tr}G \cdot \partial_{tr}\xi^{-1}$	$J \cdot x^{-1}$	2
Flux, isomorphic	$J_{tr}$	$J_{tr} = d_{tr}\xi \cdot dt^{-1} \cdot V^{-1}$	$x \cdot s^{-1} \cdot m^{-3}$	3
Advancement, $n$	$d_{tr}\xi_{H+/n}$	$d_{tr}\xi_{H+/n} = d_{tr}n_{H+} \cdot v_{H+}^{-1}$	mol	4 <i>n</i>
Advancement, $e$	$d_{tr}\xi_{H+/e}$	$d_{tr}\xi_{H+/e} = d_{tr}e_{H+} \cdot v_{H+}^{-1}$	C	4 <i>e</i>
Electric partial force, $e$	$F_{el/e}$	$F_{el/e} \equiv \Delta\Psi$	V	5 <i>e</i>
Electric partial force, $n$	$F_{el/n}$	$\Delta\Psi \cdot F = 96.5 \cdot \Delta\Psi$	$kJ \cdot mol^{-1}$	5 <i>n</i>
Chemical partial force, $e$	$F_{d,H+/e}$	$\Delta\mu_{H+}/F =$ $-\ln(10) \cdot RT/F \cdot \Delta pH$	V	6 <i>e</i>
at 37 °C		$= -0.06 \cdot \Delta pH$	$J \cdot C^{-1}$	
Chemical partial force, $n$	$F_{d,H+/n}$	$\Delta\mu_{H+} = -\ln(10) \cdot RT \cdot \Delta pH$	$J \cdot mol^{-1}$	6 <i>n</i>
at 37 °C		$= -5.9 \cdot \Delta pH$	$kJ \cdot mol^{-1}$	

811

812 1 to 4: An isomorphic motive entity or transformant, expressed in units  $x$ , is defined for any813 transformation, tr.  $x = \text{mol}$  or C in proton translocation.



- 814 2:  $\partial_{tr}G$  [J] is the partial Gibbs energy change in the advancement of transformation tr.
- 815 3: For  $x = C$ , flow is electric current,  $I_{el}$  [A = C·s<sup>-1</sup>], vector flux is electric current density per area,  $\mathbf{J}_{el}$ ,
- 816 and compartmental flux is electric current density per volume,  $I_{el}$  [A·m<sup>-3</sup>].
- 817 4n: For a chemical reaction, the advancement of reaction r is  $d_r\xi_B = d_r n_B \cdot v_B^{-1}$  [mol]. The stoichiometric
- 818 number is  $v_B = -1$  or  $v_B = 1$ , depending on B being a product or substrate, respectively, in reaction
- 819 r involving one mole of B. The conjugated *intensive* molar quantity,  $F_{B,r} = \partial_r G / \partial_r \xi_B$  [J·mol<sup>-1</sup>], is the
- 820 chemical force of reaction or *reaction-motive* force per stoichiometric amount of B. In reaction
- 821 kinetics,  $d_r n_B$  is expressed as a volume-specific quantity, which is the partial contribution to the
- 822 total concentration change of B,  $d_r c_B = d_r n_B / V$  and  $dc_B = dn_B / V$ , respectively. In open systems with
- 823 constant volume  $V$ ,  $dc_B = d_r c_B + d_e c_B$ , where r indicates the *internal* reaction and e indicates the
- 824 *external* flux of B into the unit volume of the system. At steady state the concentration does not
- 825 change,  $dc_B = 0$ , when  $d_r c_B$  is compensated for by the external flux of B,  $d_r c_B = -d_e c_B$  (Gnaiger
- 826 1993b). Alternatively,  $dc_B = 0$  when B is held constant by different coupled reactions in which B
- 827 acts as a substrate or a product.
- 828 4e: Scalar potential difference across the mitochondrial membrane. In a scalar electric transformation
- 829 (flux of charge, *i.e.* volume-specific current, from the matrix space to the intermembrane and
- 830 extramitochondrial space) the motive force is the difference of charge (**Box 2**). The endergonic
- 831 direction of translocation is defined in **Fig. 2** as  $H^{+}_{in} \rightarrow H^{+}_{out}$ .
- 832 5n:  $F = 96.5$  (kJ·mol<sup>-1</sup>)/V.
- 833 6: The electric partial force is independent of temperature (Note 5), but the chemical partial force
- 834 depends on absolute temperature,  $T$  [K].
- 835 6e:  $RT$  is the gas constant times absolute temperature.  $\ln(10) \cdot RT / F = 59.16$  and  $61.54$  mV at 298.15
- 836 and 310.15 K (25 and 37 °C), respectively.
- 837 6n:  $\ln(10) \cdot RT = 5.708$  and  $5.938$  kJ·mol<sup>-1</sup> at 298.15 and 310.15 K (25 and 37 °C), respectively.

838

### 839 3.3. Forces and fluxes in physics and irreversible thermodynamics

840 According to its definition in physics, a potential difference and as such the

841 *protonmotive force*,  $\Delta p_{H^+}$ , is not a force *per se* (Cohen *et al.* 2008). The fundamental forces of

842 physics are distinguished from *motive forces* of statistical and irreversible thermodynamics.

843 Complementary to the attempt towards unification of fundamental forces defined in physics,

844 the concepts of Nobel laureates Lars Onsager, Erwin Schrödinger, Ilya Prigogine and Peter  
845 Mitchell (even if expressed in apparently unrelated terms) unite the diversity of *generalized* or  
846 ‘isomorphic’ *flux-force* relationships, the product of which links to the dissipation function and  
847 Second Law of thermodynamics (Schrödinger 1944; Prigogine 1967). A *motive force* is the  
848 derivative of potentially available or ‘free’ energy (exergy) per isomorphic *motive* unit (**Box 3**).  
849 Perhaps the first account of a *motive force* in energy transformation can be traced back to the  
850 Peripatetic school around 300 BC in the context of moving a lever, up to Newton’s motive force  
851 proportional to the alteration of motion (Coopersmith 2010).

852         **Vectorial and scalar forces, and fluxes:** In chemical reactions and osmotic or diffusion  
853 processes occurring in a closed heterogeneous system, such as a chamber containing isolated  
854 mitochondria, scalar transformations occur without measured spatial direction but between  
855 separate compartments (translocation between the matrix and intermembrane space) or between  
856 energetically-separated chemical substances (reactions from substrates to products). Hence, the  
857 corresponding fluxes are not vectorial but scalar, and are expressed per volume and not per  
858 membrane area (**Box 2**). The corresponding motive forces are also scalar potential *differences*  
859 across the membrane (**Table 5**), without taking into account the *gradients* across the 6 nm thick  
860 mtIM (Rich 2003).

861         **Coupling:** In energetics (ergodynamics), coupling is defined as an energy transformation  
862 fuelled by an exergonic (downhill) input process driving the advancement of an endergonic  
863 (uphill) output process. The (negative) output/input power ratio is the efficiency of a coupled  
864 energy transformation (**Box 4**). At the limit of maximum efficiency of a completely coupled  
865 system, the (negative) input power equals the (positive) output power, such that the total power  
866 approaches zero at the maximum efficiency of 1, and the process becomes fully reversible  
867 without any dissipation of exergy, *i.e.* without entropy production.

868

869

870

---

871 **Box 4: Coupling, power and efficiency, at constant temperature and pressure**

872 Energetic coupling means that two processes of energy transformation are linked such that the  
873 input power,  $P_{in}$ , is the driving element of the output power,  $P_{out}$ , and the out/input power ratio  
874 is the efficiency. In general, power is work per unit time [ $J \cdot s^{-1} = W$ ]. When describing a system  
875 with volume  $V$  without information on the internal structure, the output is defined as the *external*  
876 work (exergy) performed by the *total* system on its environment. Such a system may be open  
877 for any type of exchange, or closed and thus allowing only heat and work to be exchanged  
878 across the system boundaries. This is the classical black box approach of thermodynamics. In  
879 contrast, in a colourful compartmental analysis of *internal* energy transformations (**Fig. 2**), the  
880 system is structured and described by definition of ergodynamic compartments (with  
881 information on the heterogeneity of the system; **Box 2**) and analysis of separate parts, *i.e.* a  
882 sequence of *partial* energy transformations,  $tr$ . In general, power per unit volume,  $P_{tr}/V$  [ $W \cdot L^{-1}$ ],  
883 is the product of a volume-specific flux,  $J_{tr}$ , and its conjugated force,  $F_{tr}$ , and is closely linked  
884 to the dissipation function using the terminology of irreversible thermodynamics (Prigogine  
885 1967; Gnaiger 1993a,b). Output power of proton translocation and catabolic input power are  
886 (**Fig. 2**),

887 Output: 
$$P_{H^+,out}/V = J_{H^+,out} \cdot F_{H^+,out}$$

888 Input: 
$$P_k/V = J_{O_2,k} \cdot F_{O_2,k}$$

889  $F_{O_2,k}$  is the exergonic input force with a negative sign, and,  $F_{H^+,out}$ , is the endergonic output  
890 force with a positive sign (**Box 3**). Ergodynamic efficiency is the ratio of output/input power,  
891 or the flux ratio times force ratio (Gnaiger 1993a,b),

892 
$$\varepsilon = \frac{P_{H^+,out}}{-P_k} = \frac{J_{H^+,out}}{J_{O_2,k}} \cdot \frac{F_{H^+,out}}{-F_{O_2,k}}$$

893 The concept of incomplete coupling relates exclusively to the first term, *i.e.* the flux ratio, or  
894  $H^+_{out}/O_2$  ratio (**Fig. 1**). Likewise, respirometric definitions of the  $P_{\gg}/O_2$  ratio and biochemical

895 coupling efficiency (Section 3.2) consider flux ratios. In a completely coupled process, the  
896 power efficiency,  $\varepsilon$ , depends entirely on the force ratio, ranging from zero efficiency at an  
897 output force of zero, to the limiting output force and maximum efficiency of 1.0, when the total  
898 power of the coupled process,  $P_t = P_k + P_{H^+,out}$ , equals zero, and any net flows are zero at  
899 ergodynamic equilibrium of a coupled process. Thermodynamic equilibrium is defined as the  
900 state when all potentials (all forces) are dissipated and equilibrate towards their minima of zero.  
901 In a fully or completely coupled process, output and input fluxes are directly proportional in a  
902 fixed ratio technically defined as a stoichiometric relationship (a gear ratio in a mechanical  
903 system). Such maximal stoichiometric output/input flux ratios are considered in OXPHOS  
904 analysis as the upper limits or mechanistic  $H^+_{out}/O_2$  and  $P_{\gg}/O_2$  ratios (**Fig. 1**).

---

905  
906 **Coupled versus bound processes:** Since the chemiosmotic theory describes the  
907 mechanisms of coupling in OXPHOS, it may be interesting to ask if the electrical and chemical  
908 parts of proton translocation are coupled processes. This is not the case according to the  
909 definition of coupling. If the coupling mechanism is disengaged, the output process becomes  
910 independent of the input process, and both proceed in their downhill (exergonic) direction (**Fig.**  
911 **2**). It is not possible to physically uncouple the electrical and chemical processes, which are  
912 only *theoretically* partitioned as electrical and chemical components and can be measured  
913 separately. If partial processes are non-separable, *i.e.*, cannot be uncoupled, then these are not  
914 *coupled* but are defined as *bound* processes. The electrical and chemical parts are tightly bound  
915 partial forces of the protonmotive force, since a flux cannot be partitioned but expressed only  
916 in either an electrical or chemical isomorphic format (**Table 4**).

917

#### 918 **4. Normalization: fluxes and flows**

919 The challenges of measuring mitochondrial respiratory flux are matched by those of  
920 normalization, whereby  $O_2$  consumption may be considered as the numerator and normalization

921 as the complementary denominator, which are tightly linked in reporting the measurements in  
922 a format commensurate with the requirements of a database.

923

#### 924 4.1. Flux per chamber volume

925 When the reactor volume does not change during the reaction, which is typical for liquid  
926 phase reactions, the volume-specific flux of a chemical reaction  $r$  is the time derivative of the  
927 advancement of the reaction per unit volume,  $J_{V,B} = d_r\check{c}_B/dt \cdot V^{-1}$  [(mol·s<sup>-1</sup>)·L<sup>-1</sup>]. The rate of  
928 concentration change is  $dc_B/dt$  [(mol·L<sup>-1</sup>)·s<sup>-1</sup>], where concentration is  $c_B = n_B/V$ . It is helpful to  
929 make the subtle distinction between [(mol·s<sup>-1</sup>)·L<sup>-1</sup>] and [(mol·L<sup>-1</sup>)·s<sup>-1</sup>] for the fundamentally  
930 different quantities of volume-specific flux and rate of concentration change, which merge to a  
931 single expression only in closed systems. In open systems, external fluxes (such as O<sub>2</sub> supply)  
932 are distinguished from internal transformations (metabolic flux, O<sub>2</sub> consumption). In a closed  
933 system, external flows of all substances are zero and O<sub>2</sub> consumption (internal flow),  $I_{O_2}$   
934 [pmol·s<sup>-1</sup>], causes a decline of the amount of O<sub>2</sub> in the system,  $n_{O_2}$  [nmol]. Normalization of  
935 these quantities for the volume of the system,  $V$  [L = dm<sup>3</sup>], yields volume-specific O<sub>2</sub> flux,  $J_{V,O_2}$   
936 =  $I_{O_2}/V$  [nmol·s<sup>-1</sup>·L<sup>-1</sup>], and O<sub>2</sub> concentration, [O<sub>2</sub>] or  $c_{O_2} = n_{O_2}/V$  [nmol·mL<sup>-1</sup> = μmol·L<sup>-1</sup> = μM].  
937 Instrumental background O<sub>2</sub> flux is due to external flux into a non-ideal closed respirometer,  
938 such that total volume-specific flux has to be corrected for instrumental background O<sub>2</sub> flux,  
939 *i.e.* O<sub>2</sub> diffusion into or out of the instrumental chamber.  $J_{V,O_2}$  is relevant mainly for  
940 methodological reasons and should be compared with the accuracy of instrumental resolution  
941 of background-corrected flux, *e.g.* ±1 nmol·s<sup>-1</sup>·L<sup>-1</sup> (Gnaiger 2001). ‘Metabolic’ or catabolic  
942 indicates O<sub>2</sub> flux,  $J_{O_2,k}$ , corrected for instrumental background O<sub>2</sub> flux and chemical background  
943 O<sub>2</sub> flux due to autoxidation of chemical components added to the incubation medium.

944

945

946

947 4.2. System-specific and sample-specific normalization

948 Application of common and generally defined units is required for direct transfer of  
 949 reported results into a database. The second [s] is the *SI* unit for the base quantity *time*. It is also  
 950 the standard time-unit used in solution chemical kinetics. **Table 6** lists some conversion factors  
 951 to obtain *SI* units. The term *rate* is not sufficiently defined to be useful for a database (**Fig. 7**).  
 952 The inconsistency of the meanings of rate becomes fully apparent when considering Galileo  
 953 Galilei's famous principle, that 'bodies of different weight all fall at the same rate (have a  
 954 constant acceleration)' (Coopersmith 2010).

955 **Extensive quantities:** An extensive quantity increases proportionally with system size.  
 956 The magnitude of an extensive quantity is completely additive for non-interacting subsystems,  
 957 such as mass or flow expressed per defined system. The magnitude of these quantities depends  
 958 on the extent or size of the system (Cohen *et al.* 2008).

959

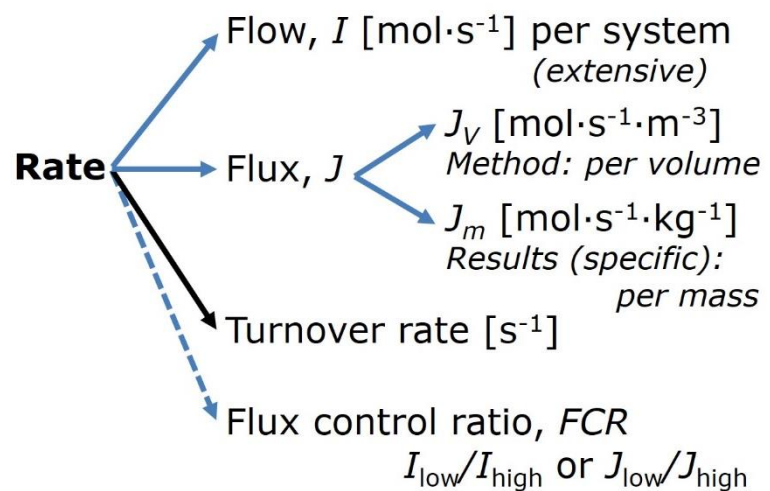
960 **Fig. 7. Different meanings of rate**

961 may lead to confusion, if the  
 962 normalization is not sufficiently  
 963 specified. Results are frequently  
 964 expressed as mass-specific flux,  $J_m$ ,  
 965 per mg protein, dry or wet weight  
 966 (mass). Cell volume,  $V_{\text{cell}}$ , or  
 967 mitochondrial volume,  $V_{\text{mt}}$ , may be  
 968 used for normalization (volume-

969 specific flux,  $J_{V_{\text{cell}}}$  or  $J_{V_{\text{mt}}}$ ), which then must be clearly distinguished from flux,  $J_V$ , expressed for  
 970 methodological reasons per volume of the measurement system, or flow per cell,  $I_x$ .

971

972 **Size-specific quantities:** 'The adjective *specific* before the name of an extensive quantity  
 973 is often used to mean *divided by mass*' (Cohen *et al.* 2008). Mass-specific flux is flow divided  
 974 by mass of the system. A mass-specific quantity is independent of the extent of non-interacting



975 homogenous subsystems. Tissue-specific quantities are of fundamental interest in comparative  
 976 mitochondrial physiology, where *specific* refers to the *type* rather than *mass* of the tissue. The  
 977 term *specific*, therefore, must be further clarified, such that tissue mass-specific, *e.g.*, muscle  
 978 mass-specific quantities are defined.

979 **Molar quantities:** ‘The adjective *molar* before the name of an extensive quantity  
 980 generally means *divided by amount of substance*’ (Cohen *et al.* 2008). The notion that all molar  
 981 quantities then become *intensive* causes ambiguity in the meaning of *molar Gibbs energy*. It is  
 982 important to emphasize the fundamental difference between normalization for amount of  
 983 substance *in a system* or for amount of motive substance *in a transformation*. When the Gibbs  
 984 energy of a system,  $G$  [J], is divided by the amount of substance B in the system,  $n_B$  [mol], a  
 985 *size-specific* molar quantity is obtained,  $G_B = G/n_B$  [J·mol<sup>-1</sup>], which is not any force at all. In  
 986 contrast, when the partial Gibbs energy change,  $\partial_r G$  [J], is divided by the motive amount of  
 987 substance B in reaction r (advancement of reaction),  $\partial_r \xi_B$  [mol], the resulting intensive molar  
 988 quantity,  $F_{B,r} = \partial G / \partial_r \xi_B$  [J·mol<sup>-1</sup>], is the chemical motive force of reaction r involving 1 mol B  
 989 (**Table 5**, Note 4).

990 **Flow per system,  $I$ :** In analogy to electrical terms, flow as an extensive quantity ( $I$ ; per  
 991 system) is distinguished from flux as a size-specific quantity ( $J$ ; per system size) (**Fig. 7**).  
 992 Electric current is flow,  $I_{el}$  [A = C·s<sup>-1</sup>] per system (extensive quantity). When dividing this  
 993 extensive quantity by system size (membrane area), a size-specific quantity is obtained, which  
 994 is electric flux (electric current density),  $J_{el}$  [A·m<sup>-2</sup> = C·s<sup>-1</sup>·m<sup>-2</sup>].

995 **Size-specific flux,  $J$ :** Metabolic O<sub>2</sub> flow per tissue increases as tissue mass is increased.  
 996 Tissue mass-specific O<sub>2</sub> flux should be independent of the size of the tissue sample studied in  
 997 the instrument chamber, but volume-specific O<sub>2</sub> flux (per volume of the instrument chamber,  
 998  $V$ ) should increase in direct proportion to the amount of sample in the chamber. Accurate  
 999 definition of the experimental system is decisive: whether the experimental chamber is the  
 1000 closed, open, isothermal or non-isothermal *system* with defined volume as part of the

1001 measurement apparatus, in contrast to the experimental *sample* in the chamber (**Table 6**).  
1002 Volume-specific O<sub>2</sub> flux depends on mass-concentration of the sample in the chamber, but  
1003 should be independent of the chamber volume. There are practical limitations to increasing the  
1004 mass-concentration of the sample in the chamber, when one is concerned about crowding  
1005 effects and instrumental time resolution.

1006 **Sample concentration  $C_{mX}$ :** Normalization for sample concentration is required for  
1007 reporting respiratory data. Consider a tissue or cells as the sample,  $X$ , and the sample mass,  $m_X$   
1008 [mg] from which a mitochondrial preparation is obtained. The sample mass,  $m_X$ , is frequently  
1009 measured as wet or dry weight,  $W_w$  or  $W_d$  [mg], or as amount of tissue or cell protein,  $m_{\text{Protein}}$ .  
1010 In the case of permeabilized tissues, cells, and homogenates, the sample concentration,  $C_{mX} =$   
1011  $m_X/V$  [ $\text{mg}\cdot\text{mL}^{-1} = \text{g}\cdot\text{L}^{-1}$ ], is simply the mass of the subsample of tissue that is transferred into  
1012 the instrument chamber. Part of the mitochondria from the tissue is lost during preparation of  
1013 isolated mitochondria, and only a fraction of mitochondria is obtained, expressed as the  
1014 mitochondrial yield (**Fig. 8**). At a high mitochondrial yield the sample of isolated mitochondria  
1015 is more representative of the total mitochondrial population than in preparations characterized  
1016 by low mitochondrial yield. Determination of the mitochondrial yield is based on measurement  
1017 of the concentration of a mitochondrial marker in the tissue homogenate,  $C_{\text{mte,thom}}$ , which  
1018 simultaneously provides information on the specific mitochondrial density in the sample (**Fig.**  
1019 **8**).

1020 Tissues can contain multiple cell populations which may have distinct mitochondrial  
1021 subtypes. Mitochondria are also in a constant state of flux due to highly dynamic fission and  
1022 fusion cycles, and can exist in multiple stages and sizes which may be altered by a range of  
1023 factors. The isolation of mitochondria (often achieved through differential centrifugation) can  
1024 therefore yield a subsample of the mitochondrial types present in a tissue, dependent on  
1025 isolation protocols utilized (*e.g.* centrifugation speed). This possible artefact should be taken  
1026 into account when planning experiments using isolated mitochondria. The tendency for



1027 mitochondria of specific sizes to be enriched at different centrifugation speeds also has the  
 1028 potential to allow the isolation of specific mitochondrial subpopulations and therefore the  
 1029 analysis of mitochondria from multiple cell lineages within a single tissue.

1030

1031 **Table 6. Sample concentrations and normalization of flux with SI/base units.**  
 1032

Expression	Symbol	Definition	SI Unit	Notes
<b>Sample</b>				
Identity of sample	$X$	Cells, animals, patients		
Number of sample entities $X$	$N_X$	Number of cells, <i>etc.</i>	x	
Mass of sample $X$	$m_X$		kg	1
Mass of entity $X$	$M_X$	$M_X = m_X \cdot N_X^{-1}$	$\text{kg} \cdot \text{x}^{-1}$	1
<b>Mitochondria</b>				
Mitochondria	mt	$X = \text{mt}$		
Amount of mt-elements	mte	Quantity of mt-marker	$x_{\text{mte}}$	
<b>Concentrations</b>				
Sample number concentration	$C_{NX}$	$C_{NX} = N_X \cdot V^{-1}$	$\text{x} \cdot \text{m}^{-3}$	2
Sample mass concentration	$C_{mX}$	$C_{mX} = m_X \cdot V^{-1}$	$\text{kg} \cdot \text{m}^{-3}$	
Mitochondrial concentration	$C_{\text{mte}}$	$C_{\text{mte}} = \text{mte} \cdot V^{-1}$	$x_{\text{mte}} \cdot \text{m}^{-3}$	3
Specific mitochondrial density	$D_{\text{mte}}$	$D_{\text{mte}} = \text{mte} \cdot m_X^{-1}$	$x_{\text{mte}} \cdot \text{kg}^{-1}$	4
Mitochondrial content, mte per entity $X$	$\text{mte}_X$	$\text{mte}_X = \text{mte} \cdot N_X^{-1}$	$x_{\text{mte}} \cdot \text{x}^{-1}$	5
<b>O<sub>2</sub> flow and flux</b>				
Flow	$I_{\text{O}_2}$	Internal flow	$\text{mol} \cdot \text{s}^{-1}$	6
Volume-specific flux	$J_{V,\text{O}_2}$	$J_{V,\text{O}_2} = I_{\text{O}_2} \cdot V^{-1}$	$\text{mol} \cdot \text{s}^{-1} \cdot \text{m}^{-3}$	7
Flow per sample entity $X$	$I_{X,\text{O}_2}$	$I_{X,\text{O}_2} = J_{V,\text{O}_2} \cdot C_{NX}^{-1}$	$\text{mol} \cdot \text{s}^{-1} \cdot \text{x}^{-1}$	8
Mass-specific flux	$J_{mX,\text{O}_2}$	$J_{mX,\text{O}_2} = J_{V,\text{O}_2} \cdot C_{mX}^{-1}$	$\text{mol} \cdot \text{s}^{-1} \cdot \text{kg}^{-1}$	9
Mitochondria-specific flux	$J_{\text{mte},\text{O}_2}$	$J_{\text{mte},\text{O}_2} = J_{V,\text{O}_2} \cdot C_{\text{mte}}^{-1}$	$\text{mol} \cdot \text{s}^{-1} \cdot x_{\text{mte}}^{-1}$	10

1033

1034 1 The SI prefix k is used for the SI base unit of mass (kg = 1,000 g). In praxis, various SI prefixes are  
 1035 used for convenience, to make numbers easily readable, e.g. 1 mg tissue, cell or mitochondrial mass  
 1036 instead of 0.000001 kg.

1037 2 In case  $X = \text{cells}$ , the sample number concentration is  $C_{N_{\text{cell}}} = N_{\text{cell}} \cdot V^{-1}$ , and volume may be expressed  
 1038 in [ $\text{dm}^3 = \text{L}$ ] or [ $\text{cm}^3 = \text{mL}$ ]. See **Table 7** for different sample types.

1039 3 mt-concentration is an experimental variable, dependent on sample concentration: (1)  $C_{\text{mte}} = \text{mte} \cdot V^{-1}$ ;  
 1040 (2)  $C_{\text{mte}} = \text{mte}_X \cdot C_{NX}$ ; (3)  $C_{\text{mte}} = C_{mX} \cdot D_{\text{mte}}$ .

1041 4 If the amount of mitochondria, mte, is expressed as mitochondrial mass, then  $D_{\text{mte}}$  is the mass  
 1042 fraction of mitochondria in the sample. If mte is expressed as mitochondrial volume,  $V_{\text{mt}}$ , and the

1043 mass of sample,  $m_X$ , is replaced by volume of sample,  $V_X$ , then  $D_{mte}$  is the volume fraction of  
 1044 mitochondria in the sample.

1045 5  $mte_X = mte \cdot N_X^{-1} = C_{mte} \cdot C_{NX}^{-1}$ .

1046 6 Entity  $O_2$  can be replaced by other chemical entities B to study different reactions.

1047 7  $l_{O_2}$  and  $V$  are defined per instrument chamber as a system of constant volume (and constant  
 1048 temperature), which may be closed or open.  $l_{O_2}$  is abbreviated for  $l_{O_2,r}$ , *i.e.* the metabolic or internal  
 1049  $O_2$  flow of the chemical reaction  $r$  in which  $O_2$  is consumed, hence the negative stoichiometric  
 1050 number,  $v_{O_2} = -1$ .  $l_{O_2,r} = d_r n_{O_2} / dt \cdot v_{O_2}^{-1}$ . If  $r$  includes all chemical reactions in which  $O_2$  participates,  
 1051 then  $d_r n_{O_2} = dn_{O_2} - d_e n_{O_2}$ , where  $dn_{O_2}$  is the change in the amount of  $O_2$  in the instrument chamber  
 1052 and  $d_e n_{O_2}$  is the amount of  $O_2$  added externally to the system. At steady state, by definition  $dn_{O_2} = 0$ ,  
 1053 hence  $d_r n_{O_2} = -d_e n_{O_2}$ .

1054 8  $J_{V,O_2}$  is an experimental variable, expressed per volume of the instrument chamber.

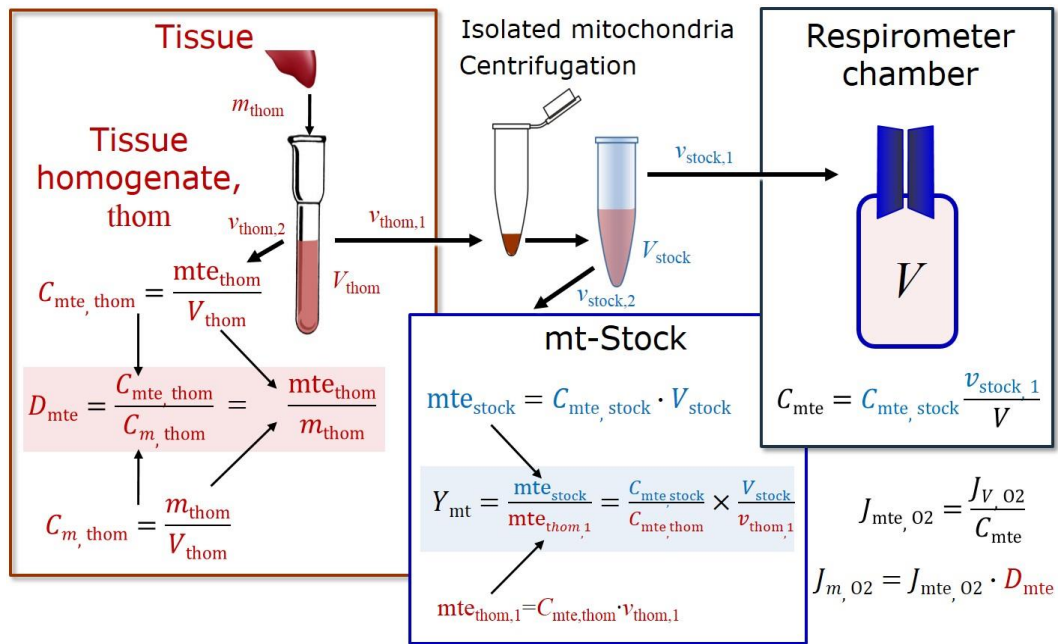
1055 9  $I_{X,O_2}$  is a physiological variable, depending on the size of entity  $X$ .

1056 10 There are many ways to normalize for a mitochondrial marker, that are used in different experimental  
 1057 approaches: (1)  $J_{mte,O_2} = J_{V,O_2} \cdot C_{mte}^{-1}$ ; (2)  $J_{mte,O_2} = J_{V,O_2} \cdot C_{mX}^{-1} \cdot D_{mte}^{-1} = J_{mX,O_2} \cdot D_{mte}^{-1}$ ; (3)  $J_{mte,O_2} =$   
 1058  $J_{V,O_2} \cdot C_{mX}^{-1} \cdot mte_X^{-1} = I_{X,O_2} \cdot mte_X^{-1}$ ; (4)  $J_{mte,O_2} = l_{O_2} \cdot mte^{-1}$ .

1059

1060 **Mass-specific flux,  $J_{mX,O_2}$ :** Mass-specific flux is obtained by expressing respiration per  
 1061 mass of sample,  $m_X$  [mg].  $X$  is the type of sample, *e.g.*, tissue homogenate, permeabilized fibres  
 1062 or cells. Volume-specific flux is divided by mass concentration of  $X$ ,  $J_{mX,O_2} = J_{V,O_2} / C_{mX}$ ; or flow  
 1063 per cell is divided by mass per cell,  $J_{mcell,O_2} = I_{cell,O_2} / M_{cell}$ . If mass-specific  $O_2$  flux is constant  
 1064 and independent of sample size (expressed as mass), then there is no interaction between the  
 1065 subsystems. A 1.5 mg and a 3.0 mg muscle sample respire at identical mass-specific flux.  
 1066 Mass-specific  $O_2$  flux, however, may change with the mass of a tissue sample, cells or isolated  
 1067 mitochondria in the measuring chamber, in which case the nature of the interaction becomes an  
 1068 issue. Optimization of cell density and arrangement is generally important and particularly in  
 1069 experiments carried out in wells, considering the confluency of the cell monolayer or clumps  
 1070 of cells (Salabei *et al.* 2014).

1071



1072

Symbol	Definition [Units]
$C_{mte}$	Mitochondrial concentration in chamber [ $x_{mte} \cdot L^{-1}$ ]
$C_m$	Sample mass concentration in chamber [ $g \cdot L^{-1}$ ]
$D_{mte}$	Specific mte-density per tissue mass [ $x_{mte} \cdot g^{-1}$ ]
$J_{m,O_2}$	Mass-specific $O_2$ flux [ $nmol \cdot s^{-1} \cdot g^{-1}$ ]
$J_{mte,O_2}$	Mitochondria-specific $O_2$ flux [ $nmol \cdot s^{-1} \cdot x_{mte}^{-1}$ ]
$mte$	Amount of mitochondrial elements [ $x_{mte}$ ]
$m_{thom}$	Mass of tissue in the homogenate [g]
$Y_{mt}$	Yield of isolated mitochondria

**Respirometer chamber**

Homogenate

$v_{thom,1}$

$V$

$$C_m = C_{m,thom} \frac{v_{thom,1}}{V}$$

$$C_{mte} = C_m \cdot D_{mte}$$

$$J_{m,O_2} = \frac{J_{V,O_2}}{C_m}$$

$$J_{mte,O_2} = \frac{J_{m,O_2}}{D_{mte}}$$

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**Fig. 8. Normalization of volume-specific flux of isolated mitochondria and tissue**

**homogenate. A:** Mitochondrial yield,  $Y_{mt}$ , in preparation of isolated mitochondria.  $v_{thom,1}$

and  $v_{stock,1}$  are the volumes transferred from the total volume,  $V_{thom}$  and  $V_{stock}$ , respectively.

$mte_{thom,1}$  is the amount of mitochondrial elements in volume  $v_{thom,1}$  used for isolation. **B:**

In respirometry with homogenate,  $v_{thom,1}$  is transferred directly into the respirometer

chamber. See **Table 6** for further explanation of symbols.

1083  
1084

**Table 7. Some useful abbreviations  
of various sample types, X.**

Identity of sample	X
Mitochondrial preparation	mtprep
Isolated mitochondria	imt
Tissue homogenate	thom
Permeabilized tissue	pti
Permeabilized fibre	pfi
Permeabilized cell	pce
Cell	ce
Organism	org

1085

1086        **Number concentration,  $C_{NX}$ :** The experimental *number concentration* of sample in the  
1087 case of cells or animals, *e.g.*, nematodes is  $C_{NX} = N_X/V$  [ $x \cdot \text{mL}^{-1}$ ], where  $N_X$  is the number of  
1088 cells or organisms in the chamber (**Table 6**).

1089        **Flow per sample entity,  $I_{X,O_2}$ :** A special case of normalization is encountered in  
1090 respiratory studies with permeabilized (or intact) cells. If respiration is expressed per cell, the  
1091  $O_2$  flow per measurement system is replaced by the  $O_2$  flow per cell,  $I_{\text{cell},O_2}$  (**Table 6**).  $O_2$  flow  
1092 can be calculated from volume-specific  $O_2$  flux,  $J_{V,O_2}$  [ $\text{nmol} \cdot \text{s}^{-1} \cdot \text{L}^{-1}$ ] (per  $V$  of the measurement  
1093 chamber [L]), divided by the number concentration of cells,  $C_{N_{ce}} = N_{ce}/V$  [ $\text{cell} \cdot \text{L}^{-1}$ ], where  $N_{ce}$   
1094 is the number of cells in the chamber. Cellular  $O_2$  flow can be compared between cells of  
1095 identical size. To take into account changes and differences in cell size, further normalization  
1096 is required to obtain cell size-specific or mitochondrial marker-specific  $O_2$  flux (Renner *et al.*  
1097 2003).

1098        The complexity changes when the sample is a whole organism studied as an experimental  
1099 model. The well-established scaling law in respiratory physiology reveals a strong interaction  
1100 of  $O_2$  consumption and individual body mass of an organism, since *basal* metabolic rate (flow)  
1101 does not increase linearly with body mass, whereas *maximum* mass-specific  $O_2$  flux,  $\dot{V}_{O_2\text{max}}$  or

1102  $\dot{V}_{O_{2peak}}$ , is approximately constant across a large range of individual body mass (Weibel and  
1103 Hoppeler 2005), with individuals, breeds, and certain species deviating substantially from this  
1104 general relationship.  $\dot{V}_{O_{2peak}}$  of human endurance athletes is 60 to 80 mL O<sub>2</sub>·min<sup>-1</sup>·kg<sup>-1</sup> body  
1105 mass, converted to  $J_{m,O_{2peak}}$  of 45 to 60 nmol·s<sup>-1</sup>·g<sup>-1</sup> (Gnaiger 2014; **Table 8**).

1106

#### 1107 *4.3. Normalization for mitochondrial content*

1108 Normalization is a problematic subject and it is essential to consider the question of the  
1109 study. If the study aims to compare tissue performance, such as the effects of a certain treatment  
1110 on a specific tissue, then normalization can be successful, using tissue mass or protein content,  
1111 for example. If the aim, however, is to find differences of mitochondrial function independent  
1112 of mitochondrial density (**Table 6**), then normalization to a mitochondrial marker is imperative  
1113 (**Fig. 9**). However, one cannot assume that quantitative changes in various markers such as  
1114 mitochondrial proteins necessarily occur in parallel with one another. It is important to first  
1115 establish that the marker chosen is not selectively altered by the performed treatment. In  
1116 conclusion, the normalization must reflect the question under investigation to reach a satisfying  
1117 answer. On the other hand, the goal of comparing results across projects and institutions  
1118 requires some standardization on normalization for entry into a databank.

1119 **Mitochondrial concentration,  $C_{mte}$ , and mitochondrial markers:** It is important that  
1120 mitochondrial concentration in the tissue and the measurement chamber be quantified, as a  
1121 physiological output and result of mitochondrial biogenesis and degradation, and as a quantity  
1122 for normalization in functional analyses. Mitochondrial organelles comprise a cellular  
1123 reticulum that is in a continual flux of fusion and fission. Hence the definition of an "amount"  
1124 of mitochondria is often misconceived: mitochondria cannot be counted as a number of  
1125 occurring elements. Therefore, quantification of the "amount" of mitochondria depends on  
1126 measurement of chosen mitochondrial markers. 'Mitochondria are the structural and functional  
1127 elemental units of cell respiration' (Gnaiger 2014). The quantity of a mitochondrial marker can

1128 be considered as the measurement of the amount of *elemental mitochondrial units* or  
 1129 *mitochondrial elements*, mte. However, since mitochondrial quality changes under certain  
 1130 stimuli, particularly in mitochondrial dysfunction and after exercise training (Pesta *et al.* 2011;  
 1131 Campos *et al.* 2017), some markers can vary while other markers are unchanged. (1)  
 1132 Mitochondrial volume and membrane area are structural markers, whereas mitochondrial  
 1133 protein mass is frequently used as a marker for isolated mitochondria. (2) Molecular and  
 1134 enzymatic mitochondrial markers (amounts or activities) can be selected as matrix markers,  
 1135 *e.g.*, citrate synthase activity, mtDNA; mtIM-markers, *e.g.*, cytochrome *c* oxidase activity, *aa*<sub>3</sub>  
 1136 content, cardiolipin, or mtOM-markers, *e.g.*, TOM20. (3) Extending the measurement of  
 1137 mitochondrial marker enzyme activity to mitochondrial pathway capacity, measured as ET- or  
 1138 OXPHOS-capacity, can be considered as an integrative functional mitochondrial marker.

1139 Depending on the type of mitochondrial marker, the mitochondrial elements, mte, are  
 1140 expressed in marker-specific units. Although concentration and density are used synonymously  
 1141 in physical chemistry, it is recommended to distinguish *experimental mitochondrial*  
 1142 *concentration*,  $C_{\text{mte}} = \text{mte}/V$  and *physiological mitochondrial density*,  $D_{\text{mte}} = \text{mte}/m_X$ . Then  
 1143 mitochondrial density is the amount of mitochondrial elements per mass of tissue (**Fig. 9**). The  
 1144 former is mitochondrial density multiplied by sample mass concentration,  $C_{\text{mte}} = D_{\text{mte}} \cdot C_{mX}$ , or  
 1145 mitochondrial content multiplied by sample number concentration,  $C_{\text{mte}} = \text{mte}_X \cdot C_{NX}$  (**Table 6**).

1146 **Mitochondria-specific flux,  $J_{\text{mte},\text{O}_2}$** : Volume-specific metabolic O<sub>2</sub> flux depends on: (1)  
 1147 the sample concentration in the volume of the instrument chamber,  $C_{mX}$ , or  $C_{NX}$ ; (2) the  
 1148 mitochondrial density in the sample,  $D_{\text{mte}} = \text{mte}/m_X$  or  $\text{mte}_X = \text{mte}/N_X$ ; and (3) the specific  
 1149 mitochondrial activity or performance per elemental mitochondrial unit,  $J_{\text{mte},\text{O}_2} = J_{V,\text{O}_2}/C_{\text{mte}}$   
 1150 (**Table 6**). Obviously, the numerical results for  $J_{\text{mte},\text{O}_2}$  vary according to the type of  
 1151 mitochondrial marker chosen for measurement of mte and  $C_{\text{mte}} = \text{mte}/V$ .

<b>Flow, Performance</b>	=	<b>Element function</b>	x	<b>Element density</b>	x	<b>Size of entity</b>
$\frac{\text{mol}\cdot\text{s}^{-1}}{x}$	=	$\frac{\text{mol}\cdot\text{s}^{-1}}{x_{\text{mte}}}$	·	$\frac{x_{\text{mte}}}{\text{kg}}$	·	$\frac{\text{kg}}{x}$

<b>A</b>	<b>Flow</b>	=	<b>mt-specific flux</b>	x	<b>mt-structure, functional elements</b>
	$I_{X,O_2}$	=	$J_{\text{mte},O_2}$	·	$\text{mte}_X$
					$\frac{\text{mte}_X}{M_X} \cdot M_X$

	$I_{X,O_2}$	=	$J_{\text{mte},O_2}$	·	$D_{\text{mte}}$	·	$M_X$
	$\frac{I_{X,O_2}}{M_X}$	=	$\frac{I_{X,O_2}}{\text{mte}_X}$	·	$\frac{\text{mte}_X}{M_X}$		

<b>B</b>	$I_{X,O_2}$	=	$J_{mX,O_2}$	·	$M_X$
	<b>Flow</b>	=	<b>Entity mass-specific flux</b>	x	<b>Mass of entity</b>

1152  
 1153 **Fig. 9. Structure-function analysis of performance of an**  
 1154 **organism, organ or tissue, or a cell (sample entity X). O<sub>2</sub>**  
 1155 **flow,  $I_{X,O_2}$ , is the product of performance per functional**  
 1156 **element (element function, mitochondria-specific flux),**  
 1157 **element density (mitochondrial density,  $D_{\text{mte}}$ ), and size of**  
 1158 **entity X (mass  $M_X$ ). (A) Structured analysis: performance is the**  
 1159 **product of mitochondrial function (mt-specific flux) and structure**  
 1160 **(functional elements;  $D_{\text{mte}}$  times mass of X). (B) Unstructured**  
 1161 **analysis: performance is the product of entity mass-specific flux,**  
 1162  **$J_{mX,O_2} = I_{X,O_2}/M_X = I_{O_2}/m_X$  [mol·s<sup>-1</sup>·kg<sup>-1</sup>] and size of entity,**  
 1163 **expressed as mass of X;  $M_X = m_X \cdot N_X^{-1}$  [kg·x<sup>-1</sup>]. See Table 6 for**  
 1164 **further explanation of quantities and units. Modified from Gnaiger**  
 1165 **(2014).**

#### 1167 4.4. Evaluation of mitochondrial markers

1168 Different methods are implicated in quantification of mitochondrial markers and have  
 1169 different strengths. Some problems are common for all mitochondrial markers, mte: (I)  
 1170 Accuracy of measurement is crucial, since even a highly accurate and reproducible



1171 measurement of O<sub>2</sub> flux results in an inaccurate and noisy expression normalized for a biased  
1172 and noisy measurement of a mitochondrial marker. This problem is acute in mitochondrial  
1173 respiration because the denominators used (the mitochondrial markers) are often very small  
1174 moieties whose accurate and precise determination is difficult. This problem can be avoided  
1175 when O<sub>2</sub> fluxes measured in substrate-uncoupler-inhibitor titration protocols are normalized for  
1176 flux in a defined respiratory reference state, which is used as an *internal* marker and yields flux  
1177 control ratios, *FCRs* (Fig. 7). *FCRs* are independent of any *externally* measured markers and,  
1178 therefore, are statistically very robust, considering the limitations of ratios in general (Jasienski  
1179 and Bazzaz 1999). *FCRs* indicate qualitative changes of mitochondrial respiratory control, with  
1180 highest quantitative resolution, separating the effect of mitochondrial density or concentration  
1181 on  $J_{mX,O_2}$  and  $I_{X,O_2}$  from that of function per elemental mitochondrial marker,  $J_{mte,O_2}$  (Pesta *et*  
1182 *al.* 2011; Gnaiger 2014). (2) If mitochondrial quality does not change and only the amount of  
1183 mitochondria, defined by the chosen mitochondrial marker, varies as a determinant of mass-  
1184 specific flux, any marker is equally qualified in principle; then in practice selection of the  
1185 optimum marker depends only on the accuracy and precision of measurement of the  
1186 mitochondrial marker. (3) If mitochondrial flux control ratios change, then there may not be  
1187 any best mitochondrial marker. In general, measurement of multiple mitochondrial markers  
1188 enables a comparison and evaluation of normalization for a variety of mitochondrial markers.  
1189 Evaluation of mitochondrial markers in healthy controls is insufficient for providing guidelines  
1190 for application in the diagnosis of pathological states and specific treatments.

1191 In line with the concept of the respiratory control ratio (Chance and Williams 1955a), the  
1192 most readily used normalization is that of flux control ratios and flux control factors (Gnaiger  
1193 2014). Selection of the state of maximum flux in a protocol as the reference state has the  
1194 advantages of (1) internal normalization, (2) statistical linearization of the response in the range  
1195 of 0 to 1, and (3) consideration of maximum flux for integrating a very large number of  
1196 elemental steps in the OXPHOS- or ET-pathways. This reduces the risk of selecting a functional



1197 marker that is specifically altered by the treatment or pathodology, yet increases the chance that  
1198 the highly integrative pathway is disproportionately affected, *e.g.* the OXPHOS- rather than  
1199 ET-pathway in case of an enzymatic defect in the phosphorylation-pathway. In this case,  
1200 additional information can be obtained by reporting flux control ratios based on a reference  
1201 state which indicates stable tissue-mass specific flux. Stereological determination of  
1202 mitochondrial content via two-dimensional transmission electron microscopy can have  
1203 limitations due to the dynamics of mitochondrial size (Meinild Lundby *et al.* 2017). Accurate  
1204 determination of three-dimensional volume by two-dimensional microscopy can be both time  
1205 consuming and statistically challenging (Larsen *et al.* 2012). Using mitochondrial marker  
1206 enzymes (citrate synthase activity, Complex I–IV amount or activity) for normalization of flux  
1207 is limited in part by the same factors that apply to the use of flux control ratios. Strong  
1208 correlations between various mitochondrial markers and citrate synthase activity (Reichmann  
1209 *et al.* 1985; Boushel *et al.* 2007; Mogensen *et al.* 2007) are expected in a specific tissue of  
1210 healthy subjects and in disease states not specifically targeting citrate synthase. Citrate synthase  
1211 activity is acutely modifiable by exercise (Tonkonogi *et al.* 1997; Leek *et al.* 2001). Evaluation  
1212 of mitochondrial markers related to a selected age and sex cohort cannot be extrapolated to  
1213 provide recommendations for normalization in respirometric diagnosis of disease, in different  
1214 states of development and ageing, different cell types, tissues, and species. mtDNA normalised  
1215 to nDNA via qPCR is correlated to functional mitochondrial markers including OXPHOS- and  
1216 ET-capacity in some cases (Puntschart *et al.* 1995; Wang *et al.* 1999; Menshikova *et al.* 2006;  
1217 Boushel *et al.* 2007), but lack of such correlations have been reported (Menshikova *et al.* 2005;  
1218 Schultz and Wiesner 2000; Pesta *et al.* 2011). Several studies indicate a strong correlation  
1219 between cardiolipin content and increase in mitochondrial functionality with exercise  
1220 (Menshikova *et al.* 2005; Menshikova *et al.* 2007; Larsen *et al.* 2012; Faber *et al.* 2014), but its  
1221 use as a general mitochondrial biomarker in disease remains questionable.

1222

## 1223 4.5. Conversion: units and normalization

1224 Many different units have been used to report the rate of oxygen consumption, OCR  
1225 (**Table 8**). *SI* base units provide the common reference for introducing the theoretical principles  
1226 (**Fig. 7**), and are used with appropriately chosen *SI* prefixes to express numerical data in the  
1227 most practical format, with an effort towards unification within specific areas of application  
1228 (**Table 9**). For studies of cells, we recommend that respiration be expressed, as far as possible,  
1229 as (1) O<sub>2</sub> flux normalized for a mitochondrial marker, for separation of the effects of  
1230 mitochondrial quality and content on cell respiration (this includes *FCRs* as a normalization for  
1231 a functional mitochondrial marker); (2) O<sub>2</sub> flux in units of cell volume or mass, for comparison  
1232 of respiration of cells with different cell size (Renner *et al.* 2003) and with studies on tissue  
1233 preparations, and (3) O<sub>2</sub> flow in units of attomole (10<sup>-18</sup> mol) of O<sub>2</sub> consumed by each cell in a  
1234 second [amol·s<sup>-1</sup>·cell<sup>-1</sup>], numerically equivalent to [pmol·s<sup>-1</sup>·10<sup>-6</sup> cells]. This convention allows  
1235 information to be easily used when designing experiments in which oxygen consumption must  
1236 be considered. For example, to estimate the volume-specific O<sub>2</sub> flux in an instrument chamber  
1237 that would be expected at a particular cell number concentration, one simply needs to multiply  
1238 the flow per cell by the number of cells per volume of interest. This provides the amount of O<sub>2</sub>  
1239 [mol] consumed per time [s<sup>-1</sup>] per unit volume [L<sup>-1</sup>]. At an O<sub>2</sub> flow of 100 amol·s<sup>-1</sup>·cell<sup>-1</sup> and a  
1240 cell density of 10<sup>9</sup> cells·L<sup>-1</sup> (10<sup>6</sup> cells·mL<sup>-1</sup>), the volume-specific O<sub>2</sub> flux is 100 nmol·s<sup>-1</sup>·L<sup>-1</sup> (100  
1241 pmol·s<sup>-1</sup>·mL<sup>-1</sup>).

1242 Although volume is expressed as m<sup>3</sup> using the *SI* base unit, the litre [dm<sup>3</sup>] is the basic unit  
1243 of volume for concentration and is used for most solution chemical kinetics. If one multiplies  
1244  $I_{\text{cell},\text{O}_2}$  by  $C_{\text{Ncell}}$ , then the result will not only be the amount of O<sub>2</sub> [mol] consumed per time [s<sup>-1</sup>]  
1245 in one litre [L<sup>-1</sup>], but also the change in the concentration of oxygen per second (for any volume  
1246 of an ideally closed system). This is ideal for kinetic modeling as it blends with chemical rate  
1247 equations where concentrations are typically expressed in mol·L<sup>-1</sup> (Wagner *et al.* 2011). In  
1248 studies of multinuclear cells, such as differentiated skeletal muscle cells, it is easy to determine

1249 the number of nuclei but not the total number of cells. A generalized concept, therefore, is  
 1250 obtained by substituting cells by nuclei as the sample entity. This does not hold, however, for  
 1251 enucleated platelets.

1252

1253 **Table 8. Conversion of various units used in respirometry and**  
 1254 **ergometry.**  $e$  is the number of electrons or reducing equivalents.  $z_B$  is the  
 1255 charge number of entity B.

1256

1 Unit	x	Multiplication factor	SI-Unit	Note
ng.atom O $\cdot$ s $^{-1}$	(2 e)	0.5	nmol O $_2$ $\cdot$ s $^{-1}$	
ng.atom O $\cdot$ min $^{-1}$	(2 e)	8.33	pmol O $_2$ $\cdot$ s $^{-1}$	
natom O $\cdot$ min $^{-1}$	(2 e)	8.33	pmol O $_2$ $\cdot$ s $^{-1}$	
nmol O $_2$ $\cdot$ min $^{-1}$	(4 e)	16.67	pmol O $_2$ $\cdot$ s $^{-1}$	
nmol O $_2$ $\cdot$ h $^{-1}$	(4 e)	0.2778	pmol O $_2$ $\cdot$ s $^{-1}$	
mL O $_2$ $\cdot$ min $^{-1}$ at STPD <sup>a</sup>		0.744	$\mu$ mol O $_2$ $\cdot$ s $^{-1}$	1
W = J/s at -470 kJ/mol O $_2$		-2.128	$\mu$ mol O $_2$ $\cdot$ s $^{-1}$	
mA = mC $\cdot$ s $^{-1}$	( $z_{H^+} = 1$ )	10.36	nmol H $^+$ $\cdot$ s $^{-1}$	2
mA = mC $\cdot$ s $^{-1}$	( $z_{O_2} = 4$ )	2.59	nmol O $_2$ $\cdot$ s $^{-1}$	2
nmol H $^+$ $\cdot$ s $^{-1}$	( $z_{H^+} = 1$ )	0.09649	mA	3
nmol O $_2$ $\cdot$ s $^{-1}$	( $z_{O_2} = 4$ )	0.38594	mA	3

1257

1258 1 At standard temperature and pressure dry (STPD: 0 °C = 273.15 K and 1 atm =  
 1259 101.325 kPa = 760 mmHg), the molar volume of an ideal gas,  $V_m$ , and  $V_{m,O_2}$  is  
 1260 22.414 and 22.392 L $\cdot$ mol $^{-1}$  respectively. Rounded to three decimal places, both  
 1261 values yield the conversion factor of 0.744. For comparison at NTPD (20 °C),  
 1262  $V_{m,O_2}$  is 24.038 L $\cdot$ mol $^{-1}$ . Note that the SI standard pressure is 100 kPa.

1263 2 The multiplication factor is  $10^6/(z_B \cdot F)$ .

1264 3 The multiplication factor is  $z_B \cdot F/10^6$ .

1265

## 1266 4.5. Conversion: oxygen, proton and ATP flux

1267  $J_{O_2,k}$  is coupled in mitochondrial steady states to proton cycling,  $J_{\infty H^+} = J_{H^+,out} = J_{H^+,in}$   
 1268 (**Fig. 2**).  $J_{H^+,out/n}$  and  $J_{H^+,in/n}$  [ $\text{nmol}\cdot\text{s}^{-1}\cdot\text{L}^{-1}$ ] are converted into electrical units,  $J_{H^+,out/e}$  [ $\text{mC}\cdot\text{s}^{-1}\cdot\text{L}^{-1}$   
 1269  $= \text{mA}\cdot\text{L}^{-1}$ ] =  $J_{H^+,out/n}$  [ $\text{nmol}\cdot\text{s}^{-1}\cdot\text{L}^{-1}$ ]  $\cdot F$  [ $\text{C}\cdot\text{mol}^{-1}$ ]  $\cdot 10^{-6}$  (**Table 4**). At a  $J_{H^+,out}/J_{O_2,k}$  ratio or  $H^+_{out}/O_2$   
 1270 of 20 ( $H^+_{out}/O = 10$ ), a volume-specific  $O_2$  flux of  $100 \text{ nmol}\cdot\text{s}^{-1}\cdot\text{L}^{-1}$  would correspond to a proton  
 1271 flux of  $2,000 \text{ nmol H}^+_{out}\cdot\text{s}^{-1}\cdot\text{L}^{-1}$  or volume-specific current of  $193 \text{ mA}\cdot\text{L}^{-1}$ .

$$1272 \quad J_{V,H^+out/e} [\text{mA}\cdot\text{L}^{-1}] = J_{V,H^+out/n} \cdot F \cdot 10^{-6} [\text{nmol}\cdot\text{s}^{-1}\cdot\text{L}^{-1} \cdot \text{mC}\cdot\text{nmol}^{-1}] \quad (\text{Eq. 3.1})$$

$$1273 \quad J_{V,H^+out/e} [\text{mA}\cdot\text{L}^{-1}] = J_{V,O_2} \cdot (H^+_{out}/O_2) \cdot F \cdot 10^{-6} [\text{mC}\cdot\text{s}^{-1}\cdot\text{L}^{-1} = \text{mA}\cdot\text{L}^{-1}] \quad (\text{Eq. 3.2})$$

1274

1275 **Table 9. Conversion of units with preservation of numerical values.**

Name	Frequently used unit	Equivalent unit	Note
Volume-specific flux, $J_{V,O_2}$	$\text{pmol}\cdot\text{s}^{-1}\cdot\text{mL}^{-1}$	$\text{nmol}\cdot\text{s}^{-1}\cdot\text{L}^{-1}$	1
	$\text{mmol}\cdot\text{s}^{-1}\cdot\text{L}^{-1}$	$\text{mol}\cdot\text{s}^{-1}\cdot\text{m}^{-3}$	
Cell-specific flow, $I_{O_2}$	$\text{pmol}\cdot\text{s}^{-1}\cdot 10^{-6}$ cells	$\text{amol}\cdot\text{s}^{-1}\cdot\text{cell}^{-1}$	2
	$\text{pmol}\cdot\text{s}^{-1}\cdot 10^{-9}$ cells	$\text{zmol}\cdot\text{s}^{-1}\cdot\text{cell}^{-1}$	
Cell number concentration, $C_{Nce}$	$10^6$ cells $\cdot\text{mL}^{-1}$	$10^9$ cells $\cdot\text{L}^{-1}$	
Mitochondrial protein concentration, $C_{mte}$	$0.1 \text{ mg}\cdot\text{mL}^{-1}$	$0.1 \text{ g}\cdot\text{L}^{-1}$	
Mass-specific flux, $J_{m,O_2}$	$\text{pmol}\cdot\text{s}^{-1}\cdot\text{mg}^{-1}$	$\text{nmol}\cdot\text{s}^{-1}\cdot\text{g}^{-1}$	4
Catabolic power, $P_{O_2,k}$	$\mu\text{W}\cdot 10^{-6}$ cells	$\text{pW}\cdot\text{cell}^{-1}$	1
Volume	1,000 L	$\text{m}^3$ (1,000 kg)	
	L	$\text{dm}^3$ (kg)	
	mL	$\text{cm}^3$ (g)	
	$\mu\text{L}$	$\text{mm}^3$ (mg)	
	fL	$\mu\text{m}^3$ (pg)	
Amount of substance concentration	$\text{M} = \text{mol}\cdot\text{L}^{-1}$	$\text{mol}\cdot\text{dm}^{-3}$	

1276

1277 1 pmol: picomole =  $10^{-12}$  mol1278 2 amol: attomole =  $10^{-18}$  mol1279 3 zmol: zeptomole =  $10^{-21}$  mol1280 4 nmol: nanomole =  $10^{-9}$  mol

1281

1282 ET-capacity in various human cell types including HEK 293, primary HUVEC and fibroblasts  
 1283 ranges from 50 to  $180 \text{ amol}\cdot\text{s}^{-1}\cdot\text{cell}^{-1}$ , measured in intact cells in the noncoupled state (see  
 1284 Gnaiger 2014). At  $100 \text{ amol}\cdot\text{s}^{-1}\cdot\text{cell}^{-1}$  corrected for ROX (corresponding to a catabolic power  
 1285 of  $-48 \text{ pW}\cdot\text{cell}^{-1}$ ), the current across the mt-membranes,  $I_e$ , approximates  $193 \text{ pA}\cdot\text{cell}^{-1}$  or 0.2

1286 nA per cell. See Rich (2003) for an extension of quantitative bioenergetics from the molecular  
 1287 to the human scale, with a transmembrane proton flux equivalent to 520 A in an adult at a  
 1288 catabolic power of -110 W. Modelling approaches illustrate the link between proton motive  
 1289 force and currents (Willis *et al.* 2016). For NADH- and succinate-linked respiration, the  
 1290 mechanistic P<sub>»</sub>/O<sub>2</sub> ratio (referring to the full 4 electron reduction of O<sub>2</sub>) is calculated at 20/3.7  
 1291 and 12/3.7, respectively (Eq. 4) equal to 5.4 and 3.3. The classical P<sub>»</sub>/O ratios (referring to the  
 1292 2 electron reduction of 0.5 O<sub>2</sub>) are 2.7 and 1.6 (Watt *et al.* 2010), in direct agreement with the  
 1293 measured P<sub>»</sub>/O ratio for succinate of 1.58 ± 0.02 (Gnaiger *et al.* 2000; for detailed reviews see  
 1294 Wikström and Hummer 2012; Sazanov 2015),

$$1295 \quad P_{\gg}/O_2 = (H^+_{out}/O_2)/(H^+_{in}/P_{\gg}) \quad (\text{Eq. 4})$$

1296 In summary (**Fig. 1**),

$$1297 \quad J_{V,P_{\gg}} [\text{nmol}\cdot\text{s}^{-1}\cdot\text{L}^{-1}] = J_{V,O_2} \cdot (H^+_{out}/O_2)/(H^+_{in}/P_{\gg}) \quad (\text{Eq. 5.1})$$

$$1298 \quad J_{V,P_{\gg}} [\text{nmol}\cdot\text{s}^{-1}\cdot\text{L}^{-1}] = J_{V,O_2} \cdot (P_{\gg}/O_2) \quad (\text{Eq. 5.2})$$

1299 We consider isolated mitochondria as powerhouses and proton pumps as molecular machines  
 1300 to relate experimental results to energy metabolism of the intact cell. The cellular P<sub>»</sub>/O<sub>2</sub> based  
 1301 on oxidation of glycogen is increased by the glycolytic (fermentative) substrate-level  
 1302 phosphorylation of 3 P<sub>»</sub>/Glyc, *i.e.*, 0.5 mol P<sub>»</sub> for each mol O<sub>2</sub> consumed in the complete  
 1303 oxidation of a mol glycosyl unit (Glyc). Adding 0.5 to the mitochondrial P<sub>»</sub>/O<sub>2</sub> ratio of 5.4  
 1304 yields a bioenergetic cell physiological P<sub>»</sub>/O<sub>2</sub> ratio close to 6. Two NADH equivalents are  
 1305 formed during glycolysis and transported from the cytosol into the mitochondrial matrix, either  
 1306 by the malate-aspartate shuttle or by the glycerophosphate shuttle resulting in different  
 1307 theoretical yield of ATP generated by mitochondria, the energetic cost of which potentially  
 1308 must be taken into account. Considering also substrate-level phosphorylation in the TCA cycle,  
 1309 this high P<sub>»</sub>/O<sub>2</sub> ratio not only reflects proton translocation and OXPHOS studied in isolation,  
 1310 but integrates mitochondrial physiology with energy transformation in the living cell (Gnaiger  
 1311 1993a).

1312

1313 **5. Conclusions**

1314 MitoEAGLE can serve as a gateway to better diagnose mitochondrial respiratory defects  
1315 linked to genetic variation, age-related health risks, sex-specific mitochondrial performance,  
1316 lifestyle with its effects on degenerative diseases, and thermal and chemical environment. The  
1317 present recommendations on coupling control states and rates, linked to the concept of the  
1318 protonmotive force (Part 1) will be extended in a series of reports on pathway control of  
1319 mitochondrial respiration, respiratory states in intact cells, and harmonization of experimental  
1320 procedures.

1321

---

**1322 Box 5: Mitochondrial and cell respiration**

1323 Mitochondrial and cell respiration is the process of highly exergonic and exothermic energy  
1324 transformation in which scalar redox reactions are coupled to vectorial ion translocation across  
1325 a semipermeable membrane, which separates the small volume of a bacterial cell or  
1326 mitochondrion from the larger volume of its surroundings. The electrochemical exergy can be  
1327 partially conserved in the phosphorylation of ADP to ATP or in ion pumping, or dissipated in  
1328 an electrochemical short-circuit. Respiration is thus clearly distinguished from fermentation as  
1329 the counterpart of cellular core energy metabolism. Respiration is separated in mitochondrial  
1330 preparations from the partial contribution of fermentative pathways of the intact cell. According  
1331 to this definition, residual oxygen consumption, as measured after inhibition of mitochondrial  
1332 electron transfer, does not belong to the class of catabolic reactions and is, therefore, subtracted  
1333 from total oxygen consumption to obtain baseline-corrected respiration.

1334

---

1335 The optimal choice for expressing mitochondrial and cell respiration (**Box 5**) as O<sub>2</sub> flow  
1336 per biological system, and normalization for specific tissue-markers (volume, mass, protein)  
1337 and mitochondrial markers (volume, protein, content, mtDNA, activity of marker enzymes,

1338 respiratory reference state) is guided by the scientific question under study. Interpretation of  
1339 the obtained data depends critically on appropriate normalization, and therefore reporting rates  
1340 merely as  $\text{nmol}\cdot\text{s}^{-1}$  is discouraged, since it restricts the analysis to intra-experimental  
1341 comparison of relative (qualitative) differences. Expressing  $\text{O}_2$  consumption per cell may not  
1342 be possible when dealing with tissues. For studies with mitochondrial preparations, we  
1343 recommend that normalizations be provided as far as possible: (1) on a per cell basis as  $\text{O}_2$  flow  
1344 (a biophysical normalization); (2) per g cell or tissue protein, or per cell or tissue mass as mass-  
1345 specific  $\text{O}_2$  flux (a cellular normalization); and (3) per mitochondrial marker as mt-specific flux  
1346 (a mitochondrial normalization). With information on cell size and the use of multiple  
1347 normalizations, maximum potential information is available (Renner *et al.* 2003; Wagner *et al.*  
1348 2011; Gnaiger 2014). When using isolated mitochondria, mitochondrial protein is a frequently  
1349 applied mitochondrial marker, the use of which is basically restricted to isolated mitochondria.  
1350 Mitochondrial markers, such as citrate synthase activity as an enzymatic matrix marker, provide  
1351 a link to the tissue of origin on the basis of calculating the mitochondrial yield, *i.e.*, the fraction  
1352 of mitochondrial marker obtained from a unit mass of tissue.

1353

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1359

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